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Brain network pathophysiology in dystonia

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Dystonia is increasingly recognized as a disorder of brain networks. This review integrates multimodal evidence from human studies to characterize the network-level pathophysiology of dystonia. Structural MRI studies using voxel-based morphometry and diffusion imaging reveal alterations in gray matter volume and white matter connectivity across the sensorimotor cortex, basal ganglia, cerebellum, and thalamus. Functional imaging modalities, including PET, fMRI, EEG, MEG, and fNIRS, demonstrate aberrant activity and connectivity in cortico-striato-pallido-thalamocortical and cerebello-thalamocortical loops. Invasive electrophysiological recordings from deep brain stimulation (DBS) provide high-resolution insights into abnormal oscillatory activity and effective connectivity within these circuits. Non-invasive brain stimulation (NIBS) techniques such as TMS, TES, and TUS provide a means of actively interrogating those networks through transient perturbation. They also provide an avenue for personalized neuromodulation. Computational models, including The Virtual Brain platform, enable integration

of multimodal data to simulate dynamic network behavior. Across focal, generalized, and genetic forms of dystonia, shared patterns of network dysfunction are observed, though phenotypic and genotypic subtypes exhibit distinct topographies and circuit-level alterations. These findings underscore the importance of network dysfunction underlying dystonia. This network perspective informs the development of more targeted and individualized diagnostic and therapeutic approaches, including circuit-guided neuromodulation and closed-loop brain stimulation. Advancing multimodal and integrative methodologies will be essential to unraveling the complex dynamics underlying dystonia and translating mechanistic insights into precision interventions.

KEYWORDS**brain networks, DBS, dystonia, MRI, PET**

Introduction

The current view of how the brain functions is that of networks. Networks play a key role in human brain function. The original movement away from a phrenology view came from the German school at the end of the 19th century and the beginning of the 20th century with Broca's and Wernicke's studies of language and aphasia and Liepmann's studies of movement and apraxia [1]. They stressed the importance of information flowing from one part of the brain to another underlying function. This view was attacked by the British school, including persons such as Head, calling these neurologists "diagram makers" and adopting a more gestalt view of brain function. Geschwind [2, 3] in a game-changing two-part paper in *Brain* in 1965, brought back the idea of the importance of brain connections to understand normal function and pathophysiology, and, stimulated by advances in MRI and EEG [4], networks have become the predominant model once again.

Increasing data demonstrate that normal movement depends on network function. Similarly, the pathophysiology of disordered movements reflects dysfunction at the network level [5]. This approach provides a basis for understanding the pathophysiology of dystonia.

Dystonia is defined as a "movement disorder characterized by sustained or intermittent abnormal movements, postures, or both" [6]. There are many syndromes of dystonia (axis 1) and many etiologies (axis 2). The pathophysiology of the movement disorder, however, appears to have similarities across this wide spectrum. While it is always optimal to treat the etiology of a disorder since that might eradicate it completely, when this is not possible, it is still often achievable to treat the symptoms. Understanding the network dysfunction, therefore, is not only useful in improving general knowledge about dystonia but also helpful for development of symptomatic treatment. Indeed, this is already clearly the case, since dystonia can be responsive to DBS whose mechanism of action includes brain circuit modification [7].

Studies of the pathophysiology of dystonia over the last several decades have revealed some fundamental abnormalities [8, 9]. The notion that dystonia is a network disorder dates back to at least the 1990s [10, 11] and continues to the current decade [12]. The motor network in particular has been suggested [13], and motor dysfunction in dystonia is often manifest as co-contraction of agonist and antagonist muscles [14]. There is also a loss of reciprocal inhibition at multiple levels, including in the spinal cord [15], in the brainstem in the form of enhanced blink reflex recovery [16], and in the motor cortex [17, 18]. One specific type of inhibition lost is surround inhibition, which predisposes to overflow movement and loss of selective motor control. In addition to overt abnormalities in the motor system, subtle abnormalities also affect the sensory system, including abnormal blood flow responses to vibratory stimulation [19, 20]. There are also abnormalities of brain plasticity with slow motor learning, some types of exaggerated plasticity, and loss of homeostatic plasticity [9]. These various physiological abnormalities, presumably resulting from brain miswiring and/or dysfunction of neurotransmitters such as GABA and dopamine and arising from genetic and environmental factors [21], are likely associated with brain network dysfunction.

This review focuses on multimodal evidence in humans of brain network dysfunction and how it might be ameliorated. Other recent reviews also cover network dysfunction in dystonia, though they exclude genetic etiologies and include rodent models [22] or focus on how DBS has provided insights into the brain networks and physiological mechanisms that underlie motor control, covering not only dystonia but also Parkinson's disease with substantial attention to animal models [23].

Organizational overview

A multitude of methods exist for studying brain networks in dystonia. In this review, we have organized them into four main categories: non-invasive brain imaging, invasive brain recordings

associated with DBS, non-invasive brain stimulation, and models of brain network dysfunction.

The first part of the review summarizes results from non-invasive brain imaging, the primary measures of network activity currently available for use in humans. The imaging modalities include 1) computed tomography (e.g., for lesions); 2) structural MRI, involving information about grey matter structures from voxel-based morphometry and white matter pathways from diffusion MRI; 3) functional near-infrared spectroscopy (fNIRS), 4) positron emission tomography (PET), including metabolic patterns and the functions of neurotransmitters such as dopamine, GABA, and acetylcholine (Ach); and 5) functional MRI (fMRI), including both resting-state and task-related conditions; and 6) EEG.

The second part of the review summarizes results from invasive brain recordings associated with DBS. Compared to brain imaging methods, recordings during and after DBS surgery enable measures of brain activity with much higher spatial and temporal precision. The temporal precision enables analyses of stimulus-evoked responses and pathological synchronized oscillations hypothesized to play a role in the network pathophysiology. However, these recordings are generally limited to only those locations in the brain that are clinically indicated. Nevertheless, combining imaging enables a broader assay of network effects, and there is increasing use of recordings made simultaneously in multiple DBS targets.

The third part of the review summarizes results from non-invasive brain stimulation (NIBS). These include many applications of TMS and TES that have been explicitly designed to normalize the hallmarks of dystonia pathophysiology by decreasing excitation, increasing inhibition, and modulating abnormal plasticity. Another NIBS method more recently explored in dystonia is transcranial ultrasound stimulation (TUS). All the NIBS modalities could be optimized for each patient by leveraging the various recording modalities, and in some cases (e.g., with EEG, TMS, and TES), this can be done on-line in a closed loop.

The fourth part of the review highlights models for brain network dysfunction in dystonia. Historically, brain network models were constrained in their level of detail and breadth of scope by limitations of computational resources. Continuing advances in computing technologies have dramatically expanded those boundaries, as evidenced, for example, by recent developments of The Virtual Brain (TVB), an informatics platform to simulate whole brain dynamics. Although it is designed to work at the gross level of mean-field dynamics, this spatial level of abstraction is a good match for a large body of prior and ongoing experimental work with brain imaging measures.

The fifth part of the review outlines future directions for applied research into network pathophysiology of dystonia. It points out methodological and analytic standards that could strengthen interpretation of future imaging studies, how

advances in DBS technology can provide novel clues about network pathophysiology, and that aspects of longitudinal and developmental dynamics on the dystonia network remain understudied. It also notes how motor behavior can provide important constraints on circuit models of the dysfunction. For example, overtrained movement patterns are thought to be a causal factor in many task-specific dystonias, and conversely properly designed physiotherapy interventions should be able to modulate the dystonic network toward normalized function. The relationships between genotype and phenotype—especially as both axes become better understood and characterized objectively—should also provide a helpful framework for understanding dystonia network pathophysiology. Finally, two specific phenotypic aspects of dystonia are highlighted as meriting more future investigation: tremor in dystonia and functional dystonia. Collectively all these research directions will help maximize what we can learn about the network pathophysiology of dystonia.

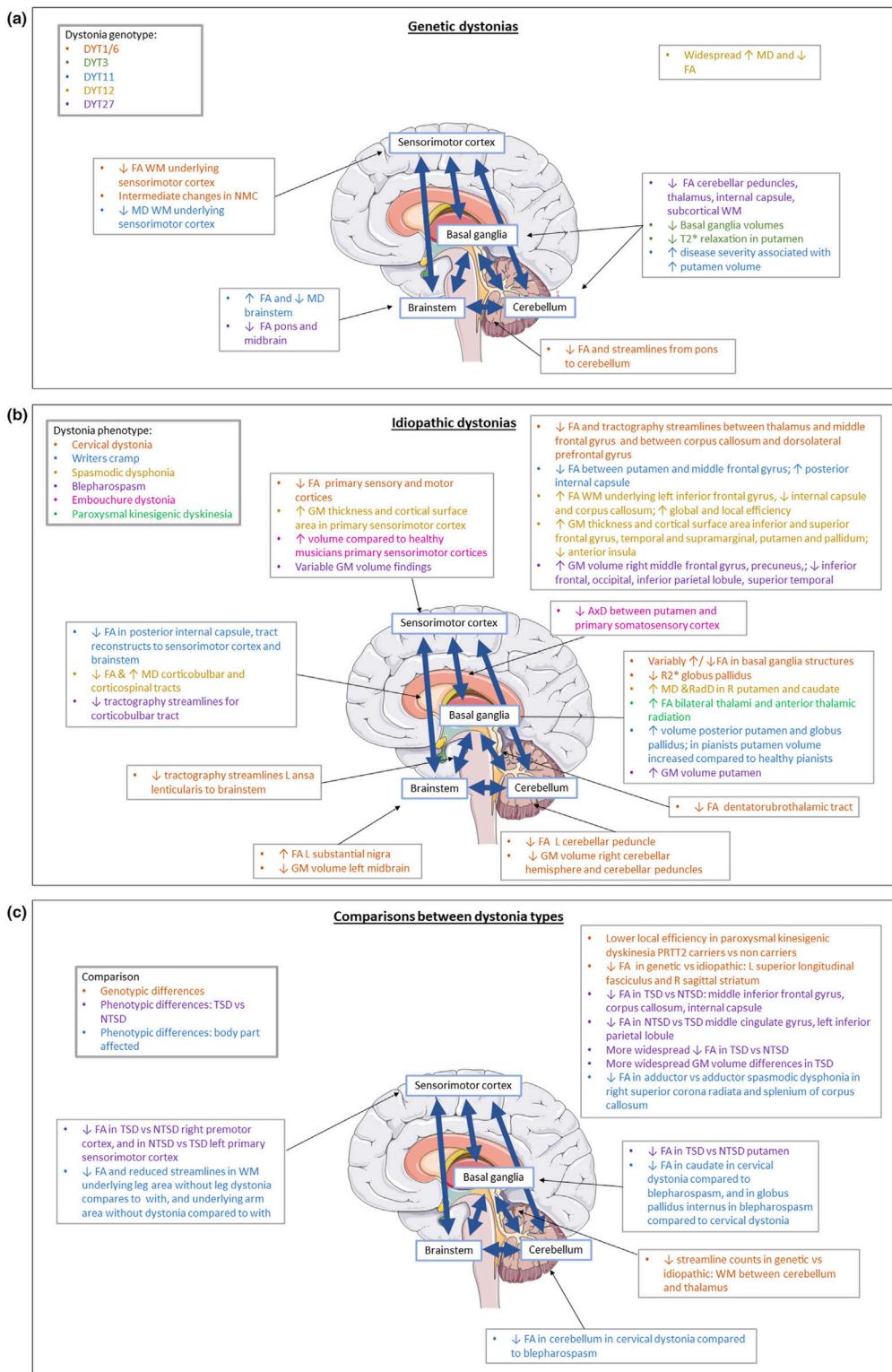
Woven throughout all parts of the review are a wide array of analytic methods, a variety of tasks, differential network findings for various dystonia subtypes defined phenomenologically and genetically, and the influence of treatments, including not only botulinum toxin (BoNT) but also DBS and TMS. Future efforts to synthesize these multiple approaches to understanding brain network dysfunction will accelerate progress toward new treatments that directly target the neural network basis of dystonia.

Non-invasive brain imaging

In routine clinical imaging, most dystonia patients exhibit no overt abnormalities [13]. Regional and network changes are generally subtle and more functional than structural: one may show abnormal function despite structurally normal scans [24]. Functional disturbances often manifest as abnormal network interactions involving basal ganglia, cerebellum, thalamus, and cortex [25]. Bhatia et al. [26] identified lesions associated with dystonia on CT and MRI; their heterogeneous locations suggested that their involvement could be accounted for with dysfunction of a network. Focal lesions may not appear on CT or MRI yet can be evident on functional imaging with PET [27].

Lesions

In dystonia, lesion-based studies most often implicate the basal ganglia and thalamus [26, 28]. Pediatric lesion-induced dystonias – including from hypoxia, kernicterus, and stroke – implicate two basal ganglia nuclei in particular: the putamen and globus pallidus (GP) [29]. These nuclei participate in the “somato-cognitive-action network” (SCAN) that involves M1 and plays a role in motor integration [30] and the

**FIGURE 1**

Summary of structural MRI differences relative to healthy controls in dystonia based on genotype, whether the phenotype is task specific, and the body parts affected for (a) genetic dystonias, (b) idiopathic dystonias, and (c) comparing the types of dystonia. FA, fractional anisotropy; GM, grey matter; WM, white matter; L, left; R, right; TSD, task- specific dystonia; NTSD, non- task- specific dystonia. Reproduced with permission from [40].

“cingulo-opercular/action-mode network” (CON/AMN) that includes the dorsal anterior cingulate and anterior insula [31], indicating that basal-ganglia injury can influence higher-order motor planning as well as execution. Cortical lesions also contribute: in BSP involving both idiopathic and acquired forms, meta-analytic connectivity modeling revealed bilateral SMA abnormalities [32]. In lesion-based CD [33], affected sites were functionally connected within a network encompassing the cerebellum, GP, striatum, midbrain, thalamus, and somatosensory cortex—a pattern likewise observed in isolated CD.

Voxel-based morphometry (VBM) and diffusion MRI

VBM quantifies local grey and white matter concentrations across the brain based on structural MRI. Diffusion MRI (dMRI) assesses water diffusion to infer the integrity and connectivity of white matter tracts linking distant regions. Together, these methods enable whole-brain assessment of structural networks, and diffusion-tractography studies have revealed differences in pathways connecting regions implicated in dystonia pathophysiology.

Structural neuroimaging studies using VBM and diffusion imaging report grey and white matter abnormalities in regions subserving motor execution and sensorimotor integration [34–36]. Although there have been differences between studies and types of isolated dystonia, common abnormalities across the subtypes may occur in sensorimotor, premotor, and parietal cortical areas, basal ganglia, thalamus, and cerebellum [37–39].

MacIver et al provided a critical analysis of methods and results from 37 volumetric and 45 dMRI studies in dystonia [40]. Regional volumetric results appeared highly variable but abnormalities in brainstem, cerebellum, basal ganglia, and sensorimotor cortex occurred most frequently (see Figure 1). Task-specific dystonias exhibited higher grey matter volume than non-task specific dystonias [38, 40]. The white matter pathways connecting implicated brain regions predominantly exhibited lower fractional anisotropy and higher mean diffusivity. Although interpretation of the higher grey matter volume remains unclear, the white matter changes suggest degraded integrity of those pathways, supporting the idea that disruptions across multiple structural connections contribute to dystonia as a network disorder. The genetic dystonias tended to have fewer cerebellothalamic tractography fiber bundles—known as “streamlines”—than the idiopathic dystonias.

Non-task specific dystonias, such as CD and BSP, were found to have more subcortical alterations, whereas task-specific dystonias, such as LD and FHD, were shown to affect cortical structures. In most studies, changes were identified in the somatotopically organized cortical regions corresponding to the body regions affected by dystonia. For instance, changes

were observed in the hand sensorimotor region in FHD [41, 42] and the face and laryngeal areas in embouchure dystonia [43] and LD [44], respectively.

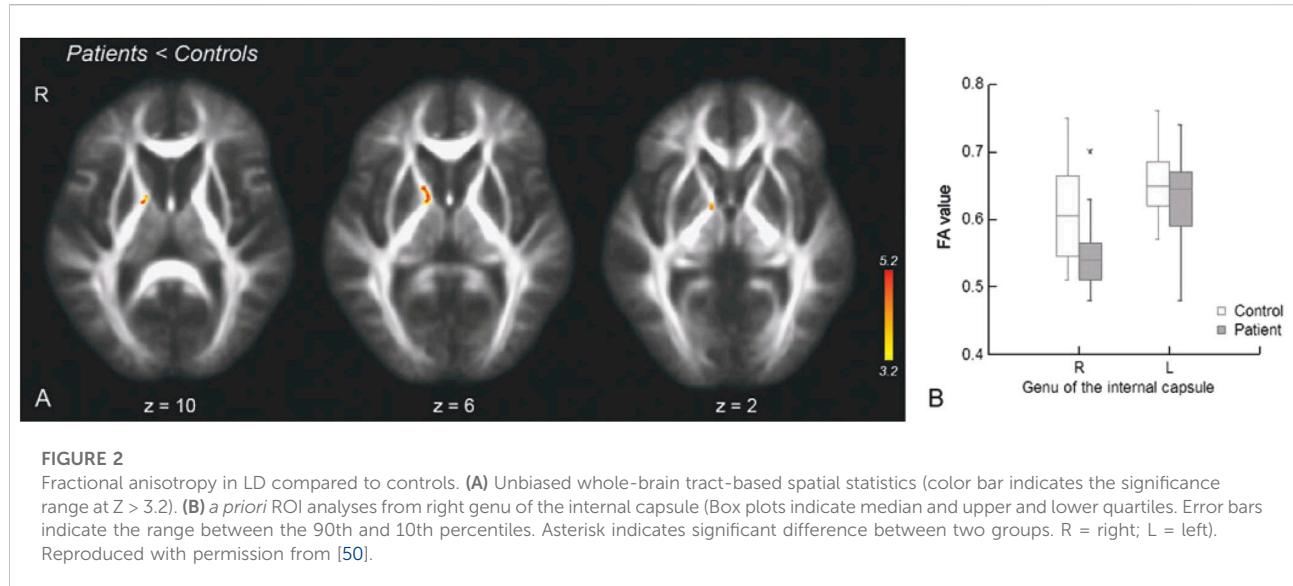
VBM

Based on VBM, dystonia exhibits distinct grey matter morphological networks because those features distinguish between dystonia and essential tremor and between dystonia and healthy controls with accuracies of 95% and 89%, respectively [45]. On the other hand, in a coordinate-based meta-analysis of 27 VBM studies in dystonia [46], no reliable grey matter volume differences were found in idiopathic dystonia. However, the authors point out that if the subtypes exhibit different volumetric profiles, the inclusion of different subtypes may have diluted the results. In CD, a multimodal meta-analysis of 9 studies [47] found differences across many brain regions, including bilateral precentral and postcentral gyri, bilateral paracentral lobules, right SMA, bilateral dorsolateral superior frontal gyri, left middle temporal gyrus, right inferior parietal gyrus, bilateral median cingulate/paracingulate gyri, lingual gyrus, right caudate, thalamus, and bilateral cerebellum. In LD, a similar multimodal analysis of 21 functional and structural neuroimaging studies, including 31 experiments in 521 LD patients and 448 healthy controls, demonstrated abnormalities in the bilateral primary motor cortices, the left inferior parietal lobule and striatum, the right insula, and the supplementary motor area [48]. In myoclonus dystonia, even the primary visual cortex has been implicated with VBM [49]. Collectively, the large number of regions involved further reinforces the view of dystonia as a network disorder and provides evidence for future investigations probing these targets with new therapies.

dMRI

dMRI changes were observed in the cortico-striato-pallido-thalamic pathway and the cerebello-thalamocortical pathway across different forms of dystonia. Among the first studies conducted with dMRI in LD patients compared to controls, decreases in white matter integrity were found along the corticobulbar/corticospinal tracts as well as in the brain regions directly or indirectly contributing to these tracts (see Figure 2) [50]. Furthermore, these neuroimaging findings were uniquely substantiated with postmortem brain pathology from a patient with LD and three controls that showed demyelination and degeneration of axonal fibers and clusters of mineral accumulations in the regions found to be abnormal on dMRI.

For BSP and CD, changes were observed in the dentato-rubro-thalamic tract, the brainstem, and the cerebellum [38, 51]. In another study, there were no differences between BSP and CD, but compared to healthy controls both patient groups exhibited fiber loss in the white matter tracts connecting GP, putamen, and thalamus with the primary sensorimotor cortex and SMA [52].



In CD, compared to healthy controls, brain networks exhibited an overall decrease of network strength and increase of local efficiency and node associativity based on graph theoretical analysis of dMRI [53]. Each group was comprised of 30 participants, and the results also held in reproducibility analyses using the Anatomical Automatic Labeling atlas. Quantitative anisotropy based on dMRI has also shown that bilateral tracts between the amygdala and the thalamus have been correlated with transient anxiety, and that bilateral tracts between the amygdala and motor, sensorimotor, and parietal association cortical areas were correlated with more persistent anxious traits [54]. Although there were no differences in TWSTRS and anxiety scales for those on vs. without anti-anxiety medications, the relative timing of the anxiety assay and the imaging were not reported.

In FHD, alterations were reported in white matter tracts connecting the putamen and the dorsal premotor cortex [55], the primary sensorimotor area [56], and the left medial frontal gyrus [57]. In embouchure dystonia, abnormalities were found in tracts connecting the putamen and the primary sensory cortex, the SMA, and the superior parietal cortex [58], and in LD, white matter alterations were described in the superior corona radiata [44].

Differences in structural connectivity based on dMRI were also explored in relationship to the clinical penetrance in carriers of DYT1 and DYT6 mutations [59]. Tractographic analysis disclosed specific changes in the integrity of cerebellothalamic (CbTC) pathways, likely of developmental origin, that regulated penetrance and variation of motor and non-motor phenotypes in these individuals [60–62]. Analogous tract changes were also identified in a knock-in mouse model [63, 64].

Taken together, these studies support the hypothesis that dystonia is a network disorder involving networks connecting the striatum, the sensorimotor and fronto-parietal cortices, and the cerebellum.

VBM and dMRI heterogeneity

Some results varied between studies and types of dystonia, raising several questions. What would be common or specific to each type of dystonia? What would be due to differences in patient characteristics or imaging protocols that varied between studies? Direct comparisons between different types of isolated dystonia reported interesting findings in this regard. Several studies suggested that the regions affected could differ between task-specific and non-task-specific dystonias using VBM [38, 65] or diffusion imaging [66]. For instance, the cerebellum and the primary sensorimotor areas were commonly affected in both task-specific (FHD and LD) and non-task-specific (BSP and CD) dystonia, whereas regions responsible for dystonic movements (i.e., writing and speaking) were specifically affected in task-specific dystonia [38]. Another study suggested that changes might differ between dystonia types with increased grey matter volume being observed in task-specific dystonia (FHD and LD) and reduced grey matter volume observed in non-task-specific dystonia (BSP and CD) [67]. Finally, some differences in brain abnormalities have also been found when stratifying patients based on their level of training, such as musician's dystonia, including musician's FHD and singer's LD, vs. non-musician's dystonia, including FHD and LD [65, 68].

In inherited dystonias, structural changes were reported as increased grey matter volume in the right GPi in patients with DYT1 mutation [69], decreased anisotropy in the motor subcortical white matter in patients with DYT1 mutation [70], and reduced cerebello-thalamocortical connectivity in patients with DYT1 and DYT6 mutations [59]. In patients with PRRT2-related paroxysmal kinesigenic dyskinesia, which can exhibit symptoms of dystonia, changes were observed in the basal ganglia cortical network, with reduced grey matter volume in

the SMA and right inferior frontal gyrus and reduced mean diffusivity in the left corticospinal tract [71], along with increased fiber density in the cerebellar pathway [72].

Another important question is the relationship between phenotype- and genotype-specific structural alterations. In LD, phenotype-specific changes were observed in the primary sensorimotor cortex and the superior corona radiata, whereas genotype-specific changes were observed in the superior temporal gyrus, the SMA, and the superior longitudinal fasciculus [44]. Two studies have suggested that differences in putaminal volume might represent an endophenotype in inherited dystonia, with increased putaminal volume in asymptomatic DYT1 carriers [73] and unaffected relatives of patients with adult-onset dystonia. The latter had displayed an abnormal temporal discrimination threshold, potentially indicating abnormal sensory processing similar to that seen in their affected relatives [74]. Similarly, putamen volume may be abnormal in people with isolated idiopathic cranial or hand dystonia [75]. Changes in the cerebello-thalamic fiber tract were common to patients with inherited and sporadic dystonias, whereas changes in the thalamocortical fiber tract were only observed in non-manifesting carriers or in non-affected regions of patients with sporadic dystonia [76].

Imaging studies during DBS procedures have also shown the importance of striatal and cerebellar circuits connected to cortical sensorimotor areas. DBS electrodes for dystonia treatment are typically placed in the postero-latero-ventral sensorimotor GPi [77, 78], a key node of the basal ganglia-cortical network. Diffusion-based connectivity between the GPi and the sensorimotor putamen predicted DBS outcomes in CD and correlated with clinical improvement [79]. Effective contacts also localized near the dentato-rubro-thalamic tract [80].

Structural imaging features can further classify dystonia subtypes. Using discriminant analysis, patients with CD and BSP could be distinguished with 100% and 83% accuracy from healthy subjects, respectively. Using more advanced deep learning, patients with LD, CD, and BSP could be distinguished with 98.8% accuracy based on an automatically identified pathophysiological neural network biomarker [81].

Limitations of structural imaging

Structural imaging studies in CD [82] and FHD [83] sometimes reported negative findings. Many were underpowered or used uncorrected statistical thresholds, yielding subtle effects. These limitations highlight the importance of studying large groups of patients with robust statistics, encouraging multicentric and international collaborations, especially for inherited rarer forms of dystonia. Because most studies are cross-sectional, they do not allow for determining whether the observed structural changes were the cause or the consequence of the disease, e.g., to dissociate pathophysiological hallmarks from compensatory mechanisms. Studies of the effect of treatment in asymptomatic carriers and

longitudinal studies—and more broadly careful alignment of study goals and designs [84]—could provide important information in this regard. The neuropathological correlates of structural imaging changes are still poorly understood. Whether they correspond to changes in cell or fiber number, shape, size, dendritic arborization, or tissue architecture is not known. This insufficient knowledge highlights the need for 1) the development of new validated imaging techniques to study *in-vivo* microstructural changes related to cellular organization (e.g., with diffusion weighted magnetic resonance spectroscopy [85]) and 2) comparative imaging and histological studies in animal models and post-mortem human tissue.

Summary of structural imaging

Despite these limitations, structural imaging consistently implicates the cortico-striato-pallido-thalamic pathway and the cerebello-thalamocortical pathway in dystonia. They also suggest that not only brain regions involved in these networks but also connections between them are abnormal [35], in line with the view of dystonia as a network disorder. The results from structural imaging also lay the foundation for evaluating the network physiology that is assayed with functional imaging.

Functional near-infrared spectroscopy (fNIRS)

Functional near-infrared spectroscopy (fNIRS) measures changes in the concentrations of oxygenated and deoxygenated hemoglobin in the cortex. FHD patients exhibit task-specific patterns in their oxygenated hemoglobin distinct from healthy controls [86]: writing increased activation in the right and left motor cortex and SMA, whereas finger tapping decreased activation in the left sensorimotor cortex and bilateral SMA.

Positron emission tomography (PET)

PET measures of metabolism

Before fMRI became widespread, PET already illuminated dystonia pathophysiology through altered metabolism and neurotransmission. In 1984, PET revealed basal ganglia dysfunction contralateral to hemidystonia in a person that had normal CT and MRI scans [27]. Later PET studies focused on metabolic brain imaging with 18F-fluorodeoxyglucose (FDG) as a marker of local synaptic activity [87, 88]. Using spatial covariance analysis [89], a reproducible dystonia-related metabolic pattern, termed DytRP, was identified in patients with genotypic and sporadic forms of the disorder [90, 91]. The DytRP network was characterized by significant contributions from the putamen, pons, cerebellum, and sensorimotor cortex. In addition to being expressed in

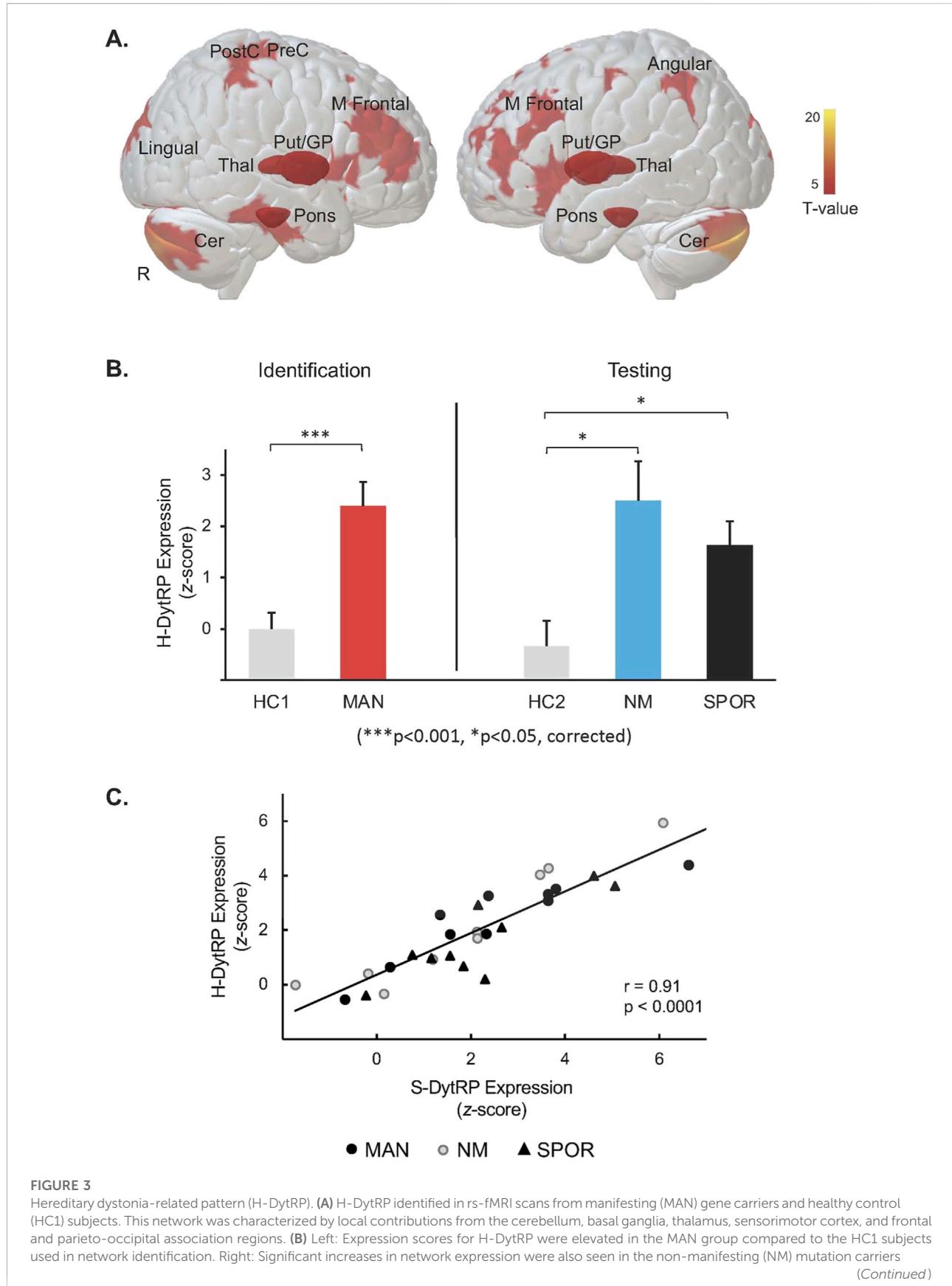


FIGURE 3 (Continued)

and patients with sporadic dystonia (SPOR) compared to HC2 testing subjects. (C) Expression values for the H-DytRP were highly correlated with corresponding subject scores for a similar sporadic dystonia-related pattern (S-DytRP) identified in an analysis of the SPOR data. (Cer, cerebellum; Put/GP, putamen/globus pallidus; Thal, thalamus; PostC, postcentral; PreC, precentral; M frontal, middle frontal). T-map thresholded at 4.8 ($P < 0.001$); color stripe. Error bars represent standard error of the mean. *** $P < 0.001$; * $P < 0.05$ relative to HC, corrected for multiple comparisons. Reproduced with permission from [192].

patients with sporadic dystonia, subject scores for this pattern were elevated to a similar degree in manifesting (MAN) and non-manifesting (NM) carriers of DYT1 and DYT6, suggesting that DytRP expression may, in certain populations, be an endophenotypic trait. Results from these PET studies served as the foundation for a “Dystonia-related pattern” subsequently evaluated with rs-fMRI (see Figure 3). Networks involving the cerebellum are also differentially affected by modulators of the GABA_A system: in FTSD, compared to placebo, Zolpidem induced hypometabolism in the right cerebellum and hypermetabolism in the left inferior parietal lobule and left cingulum [92].

PET measures of neurotransmitter systems

Neurotransmitter-specific PET studies have mostly focused on abnormalities in dopaminergic pathways—especially within the putamen, which has among the highest density of dopamine receptors in the brain. PET studies have also identified GABAergic and possible cholinergic abnormalities. Each of these neurochemical changes reflects regional contributions to the broader dystonia network.

PET studies identified functional abnormalities not easily identifiable by structural imaging, and in multiple cases implicated the putamen, hinting at possible dopaminergic dysfunction. The first demonstrated striatal (later identified as putaminal) alterations in blood flow and oxygen extraction and metabolism contralateral to the affected side of the body in an individual with post-traumatic paroxysmal hemidystonia [27]. This individual had normal anatomy as visualized by CT and MRI. With the methods available at the time, no obvious abnormalities were found in resting blood flow measures in people with isolated, idiopathic dystonia. This lack of resting-state abnormality led to a second series of observations reporting abnormalities in vibration-induced blood flow responses in sensorimotor cortex and SMA in those with unilateral, isolated, idiopathic dystonia [20] unilateral writer’s cramp [93] and cranial dystonia [94]. Interestingly these abnormalities were not only contralateral to the affected side in the limb dystonias but also in the ipsilateral side of the brain. A hint that these findings related to striatal dysfunction came from a study showing the same reduced vibration-induced blood flow that normalized after oral levodopa in participants with dopa-responsive dystonia [19]. Yet, these indirect measures did not directly prove dopaminergic dysfunction.

Direct PET measures of dopaminergic radioligands did demonstrate abnormalities in striatal dopaminergic systems.

First, patients with idiopathic, isolated cranial and hand dystonia had reduced striatal binding of a D2-like radioligand ([18F]spiperone) [10] that matched the transient reduction found in an animal model of transient dystonia induced by internal carotid infusion of the selective dopaminergic neurotoxin MPTP [10, 95]. These abnormalities were later determined to be somatotopically organized in the putamen based upon the part of the body affected by dystonia [96]. Subsequent studies confirmed these D2-like changes with a more specific radioligand, [11C]raclopride, in manifesting or nonmanifesting carriers of mutations in DYT1 or DYT6 dystonia [90, 97] as well as in those with idiopathic, isolated FHD or LD [98, 99]. These latter two studies also took advantage of [11C] raclopride, which is displaced by the release of endogenous dopamine, to demonstrate the somatotopically related abnormal phasic striatal release of dopamine in response to symptomatic and asymptomatic motor tasks. However, [18F] spiperone has specific binding to all D2-like receptors, including D2, D3, and D4 dopamine receptors. In contrast, [18F]N-methylbenperidol has a 200-fold greater affinity to D2 receptors compared to D3 or D4, and the application of [18F]N-methylbenperidol did not reveal any striatal differences in D2 receptor binding in a cohort of patients with idiopathic, isolated FHD and cranial dystonia suggesting the previously found D2-like abnormalities may be mediated by D3-specific receptors [100]. An earlier study using [11C]NNC-112, a D1-like selective radioligand also did not find striatal differences in a mixed cohort of patients with isolated hand, cranial, and cervical dystonia [101], whereas using a higher resolution scanner in better-stratified patient cohorts permitted identification of somatotopically related abnormalities in isolated FHD and LD patients [102]. Taken together, these striatal dopaminergic abnormalities were thought to represent dysfunction of the D2-mediated indirect pathway that is important for surround inhibition of unwanted movements during selected motor activity [19], while abnormalities in the D1-mediated direct pathway could reflect excessive action of the pathway important for selective motor activation [102].

Several other studies focused on GABA_A receptors using the radioligand [11C]flumazenil. One early study with a small number of participants with either DYT1 dystonia or isolated, idiopathic dystonia found reductions in sensorimotor cortex [103]. In contrast, a larger study focusing solely on isolated, idiopathic CD found higher uptake in the right precentral gyrus and left parahippocampal gyrus and no regions with significant reductions. Interestingly, decreased uptake in cerebellar

hemispheres correlated with severity, whereas decreased vermis uptake correlated with disease duration [104]. Higher [¹¹C] flumazenil uptake also occurred in those with idiopathic, isolated FHD in the inferior frontal gyrus but decreased in the cerebellar vermis [105]. Together, these findings implicate abnormalities of cerebellar GABA_A and suggest abnormalities in various cortical regions that would fit with dysfunction of cortical inhibition.

Initial studies of cholinergic function using a vesicular acetylcholinergic transport radioligand [106] indicate that posterior putamen may have lower uptake but that this may only occur in younger patients with DYT1 dystonia, while a reduction in cerebellar vermis does not depend upon age [107]. Given the functionally significant role of ACh in the striatum [108], and in particular how it modulates thalamostriatal transmission [109] and the D1- and D2-mediated pathways, PET imaging with ligands for the cholinergic system merit further investigation.

What does all of this mean, and how does it advance our understanding of network mechanisms underlying dystonia? It is likely that selective transmitter abnormalities occur in various forms of dystonia, and commonalities exist across the different forms. Such common findings include dysfunction of striatal dopaminergic systems in isolated focal, idiopathic dystonias, as well as DYT1 and DYT6 dystonias [10, 90, 95–97]. Yet, some abnormalities may be somatotopically organized, reflecting the affected body parts [98, 99, 102]. The dopamine-dependent changes in striatum are consistent with a large body of evidence pointing to a role for dopamine in mediating abnormal synaptic plasticity that could play a role in motor reinforcement learning and the corresponding development of abnormal functional circuits involving the striatum [110, 111]. The striatal dopamine system abnormalities also led to the notion of hypofunctional indirect and hyperfunctional direct basal ganglia pathways [102] with subsequent reduction of cortical inhibition consistent with abnormalities of vibration-induced blood flow responses in idiopathic, isolated dystonia [20, 93, 94] and physiologic observations of reduced cortical inhibition [112]. These data on reduced inhibition are consistent with abnormalities of GABA_A receptors in a network that mediates cortical inhibition [103–105]. Although the precise role of cholinergic systems remains to be determined, this complex network interplay likely involves brainstem nuclei, dysregulated thalamostriatal transmission, and a cascade of changes in the D1-mediated direct and D2-mediated indirect pathways through the basal ganglia. Of course, data about cerebellar dysfunction fits well with the increasing understanding of the anatomic and functional relationships between basal ganglia networks and cerebellum [113, 114], including potential relationships between the cholinergic cerebellar vermis with basal ganglia and cortical regions [115, 116].

Most importantly, multimodal studies that combine neuroimaging of transmitter systems with physiologic measures or resting-state functional connectivity will help take these investigations to the next level. For example, the specific putaminal location of a D1 receptor abnormality found with PET [102] was used as a seed for a resting-state functional connectivity study that facilitated identification of specific dysfunctional small-scale networks in people with idiopathic, isolated focal dystonias, whereas rigorous quality control measures eliminated the statistical significance of apparent large-scale, global network abnormalities [117]. Thus, advances in understanding the underlying network dysfunction related to various forms of dystonia will be facilitated by studies that combine various modalities, such as different imaging techniques and other physiologic measures.

Functional MRI (fMRI)

Functional MRI has yielded important insights into dystonia pathophysiology. It enables simultaneous assessment of distant structures at rest (rs-fMRI) or during tasks, though practical constraints can limit participation for severe generalized dystonia. Most studies focus on focal dystonia and demonstrate impaired brain-network properties.

Resting-state fMRI (rs-fMRI)

Intrinsic functional features of brain connections at rest reveal task-free properties of brain networks without the online confound of behavioral performance that may differ between populations. Compared to neurologically normal controls, patients with focal [65, 118–121] and generalized dystonias [122] show either reduced or excessive inter-regional correlations. Because these correlations depend on underlying white-matter architecture, some rs-fMRI abnormalities likely overlap with diffusion-MRI findings.

A meta-review of 46 dystonia rs-fMRI studies [123] most often implicated the sensorimotor cortex, SMA, putamen, parietal cortex, thalamus, and cerebellum, with connectivity changes primarily in the sensorimotor network [123]. Mixed directions of effect likely reflect differences in analytic choices, quality control, and cohort. While common dysfunctions may be part of a general hallmark of dystonia, dysconnectivity patterns in particular networks vary among the different forms of dystonia.

In CD in particular, a meta-analysis of 17 studies using anisotropic effect size-based signed differential mapping (AES-SDM) identified abnormalities in many regions, including bilateral precentral and postcentral gyri, bilateral paracentral lobules, right SMA, bilateral median cingulate/paracingulate gyri, right caudate nucleus and thalamus, right cerebellum and lingual gyrus, right fusiform gyrus, and bilateral precuneus [47]. Sensory network dysfunction at rest encompasses cross-modal sensory areas [124]. Sensorimotor connectivity differs by sensory

trick—decreased in patients with a trick and increased in patients without a trick [125]. Perhaps relatedly, connectivity between cortex and cerebellum decreased proportional to BoNT efficacy [126]. Furthermore, compared to healthy controls, the lower range of motion and compromised movement quality during a head “reaching task” seen in CD correlate with decreased functional connectivity among SMA, occipital cortex, and cerebellar regions [127]. In CD patients with GPi-DBS, optimal stimulator settings (compared to non-optimal and stimulator off) reduced activity in sensorimotor cortex in proportion to long-term clinical improvement, and a similar trend appeared in a few cases of generalized dystonia [123, 128].

In BSP, rs-fMRI links spasm intensity to cerebellar and sensorimotor cortical activation, and spasm onset to involvement of the basal ganglia and frontal eye field portion of the superior frontal gyrus [129].

In FHD, rs-fMRI shows distorted digit representation in the somatosensory cortex [130]. It also reveals dysfunctional cortico-subcortical circuits involving somatosensory cortex, primary and secondary motor areas, cerebellum, and basal ganglia [120, 121, 131]. Similarly in musician’s dystonia involving the hand, when compared to healthy musicians, resting state connectivity is reduced within the basal ganglia network [132] but increased in the basal ganglia associative loops with the dorsolateral prefrontal cortex and the premotor cortex [133].

In LD, rs-fMRI demonstrated abnormal functional connectivity within sensorimotor and frontoparietal networks compared to healthy individuals as well as phenotype- and genotype-distinct alterations of these networks, involving primary somatosensory, premotor, and parietal cortices [58, 118]. Battistella et al. [118] was also the first to apply a machine learning algorithm (linear discriminant analysis) to brain imaging data to show the feasibility of this approach for classifying LD patients as distinct from healthy controls with a 71% accuracy based on their differences in the connectivity measures in the left inferior parietal and sensorimotor cortices. When categorizing between different forms of LD, the combination of measures from the left inferior parietal, premotor, and right sensorimotor cortices achieved 81% discriminatory power between familial and sporadic cases, whereas the combination of measures from the right superior parietal, primary somatosensory, and premotor cortices led to 71% accuracy in the classification of adductor vs. abductor forms of LD. Although risk factors for LD remain unclear, in a study using precise demographic and clinical characterization in a large cohort of patients, environmental factors influencing sensory feedback processing explain neural alterations in the parietal, insular, and sensorimotor cortical regions [134].

In a single study involving multiple forms of focal dystonia, dysfunction of sensorimotor cortex and prefrontal division of the thalamus represented a common hallmark of task-specific focal dystonia [68]. A recurrent finding in resting-state studies is the abnormal connectivity between parietal and premotor cortices in

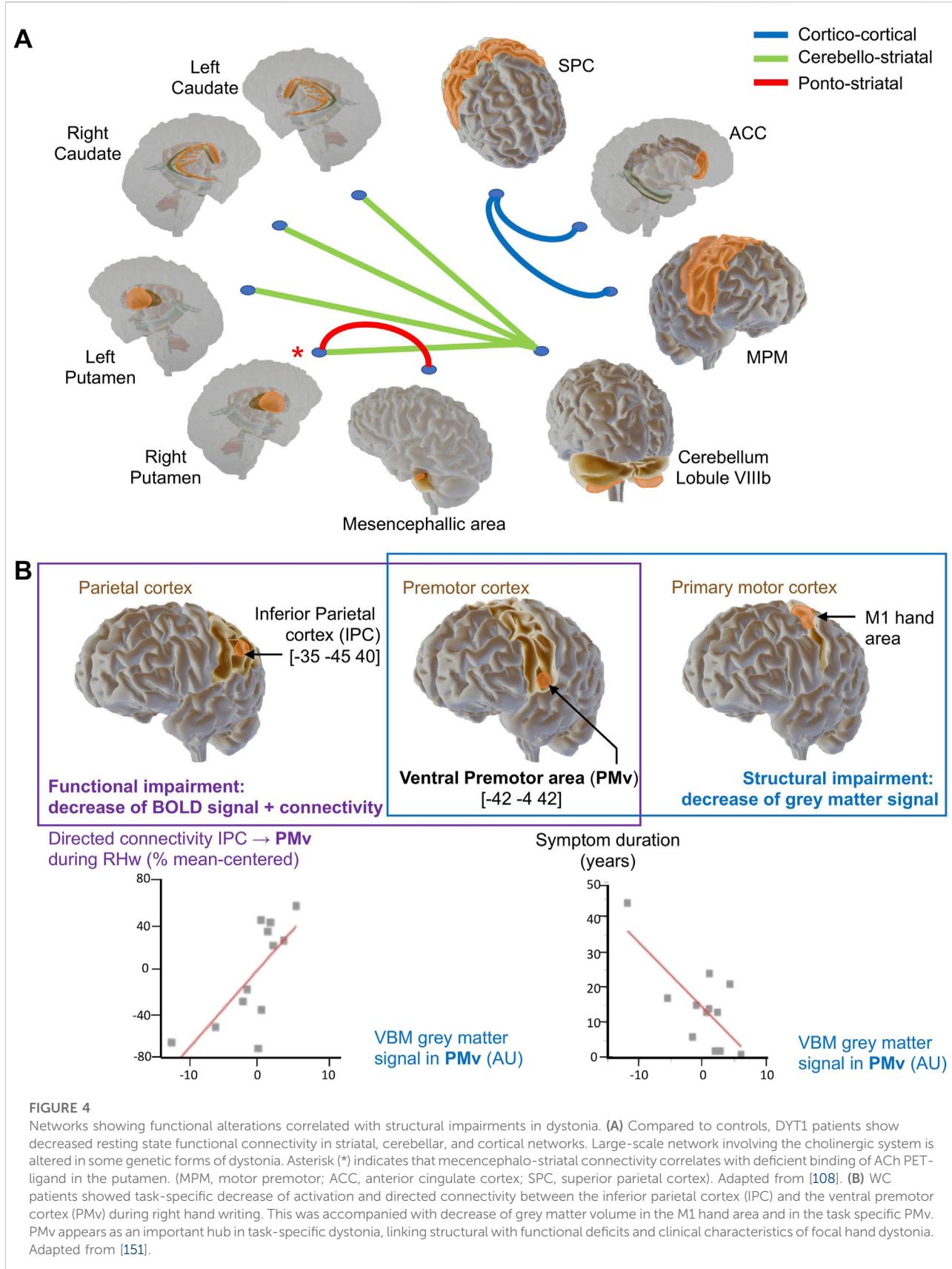
different forms of focal dystonia [65, 68, 118, 119, 135–141] and in generalized dystonia [122].

Some forms of genetic dystonia show dysfunction of cerebello-cortical and cerebello-striatal loops [72, 107]. The abnormal outputs from cerebellar cortex to deep cerebellar nuclei would in turn increase the drive of deep cerebellar nuclei to the thalamus, a mechanism that likely plays a critical role in the pathophysiology of dystonia [35]. For instance, in PRRT2 patients, abnormal cerebellar drive toward the thalamic relays of the striatum and motor cortex was partly normalized after cerebellar non-invasive stimulation compared to placebo [72]. In addition, in DYT1 patients, increase of brainstem-striatal functional connectivity was associated with the binding potential of cholinergic ligand in the striatum [107]: higher functional connectivity was associated with lower expressions of acetylcholine vesicular transporter. This suggests concomitant and interdependent functional impairments of cerebellar and striatal nodes.

Another key factor is the role of quality control for analysis of these resting state studies, as less rigor can lead to many statistically significant, yet spurious findings [117]. This is particularly important for interpretation of meta-analyses of numerous studies each of which may not apply such rigor consistently.

Task-related fMRI: motor dysfunction

Considering motor tasks, network dysfunction is present at all stages of motor control, i.e., motor planning, motor preparation, and motor execution. During task periods preceding movement onset or the imagination of hand movements, FHD patients have impaired cortical and basal ganglia activation [142, 143] that sometimes extends to the cerebellum [142]. Abnormal motor planning was often related to task-related dysfunction of parietal and lateral premotor areas during imagined movement [144, 145] and during the execution of right (symptomatic) handwriting compared to other tasks (tapping, zigzagging) performed with different limbs (left hand, right foot) [146]. In particular, an increase in practice-related activity in the premotor cortex, later associated with motor consolidation, suggests the formation of abnormal motor engrams [55]. During motor execution, hyperactivity in primary somatosensory and motor cortices were generally observed in different forms of focal dystonia [147–151], and in myoclonus dystonia [152]. For CD, BSP, and LD, task-related dysfunctions were demonstrated in cortical, cerebellum and/or basal ganglia activation during non-symptomatic tasks [82, 148, 153–156]. In the context of LD, when ADSD patients were compared to controls, cerebellar activation was reduced during symptomatic phonation and modified during the asymptomatic tasks [148, 157]. Network regions involved in different forms of dystonia for symptomatic [144, 146] and non-symptomatic [156, 158, 159] tasks may indicate that motor commands are elaborated and executed through a



common pathway that contributes importantly to the pathophysiology of dystonia (see [Figure 4](#)). A recent study showed abnormal involvement of cognitive and visual networks during rest periods interleaved with task execution [\[159\]](#). Task-related connectivity studies showed that patients with focal dystonia have changes in the strength of cortico-cortical motor and cortico-basal ganglia connections, and abnormal cerebello-thalamocortical connections [\[55, 140, 160\]](#). Task-related connectivity in dystonic hand tremor showed specific involvement of associative cortical, cerebellar and striatal regions [\[161\]](#).

Beyond parieto-premotor cortices and cerebellar regions, larger studies of focal dystonia patients ($n \geq 30$) showed altered connectivity in broader networks encompassing insular [\[162, 163\]](#) and prefrontal areas [\[164\]](#) extending the dysfunctional network to cognitive-limbic associative areas. For instance, these findings were observed during reward learning with increased activation in the anterior cingulate cortex [\[165\]](#). They were also observed when resting-state connectivity was associated with offline task performance, as abnormal communication between cerebellum and pre-SMA correlated with impaired agency (the loss of perception of control over one's action) during a visuomotor task [\[166\]](#).

Task-related fMRI: sensory dysfunction

Several paradigms allow for investigating task-related sensory dysfunction, including sensory stimulation of a body part, passive movements, and discrimination in time or space between two sensory stimuli. Patients with isolated dystonia affecting a specific body part showed an abnormal representation of the symptomatic limb in the somatosensory cortex, with excessive overlap of cortical representation of digits for writer's cramp [\[130\]](#) and of mouth for embouchure dystonia [\[167\]](#), as well as abnormal activation of lips, face, or digit areas during sensory stimulation [\[168, 169\]](#). Sensory stimulation also engaged dysfunction of the primary sensory cortex unrelated to the affected limb [\[170, 171\]](#) and other brain areas, including GPi [\[172\]](#), striatum and cerebellum [\[61, 173, 174\]](#). Dysfunction of the putamen was often observed in different forms of dystonia during tasks involving perceptual judgements [\[175–177\]](#), with dysfunction that extended to the superior colliculus in CD [\[171\]](#) and insular cortex in FHD [\[176\]](#). In LD, abnormal temporal discrimination was associated with dysfunction in the middle frontal and primary somatosensory cortices, while cerebellar and striatal dysfunctions were form (sporadic/familial)- or symptom-specific [\[178\]](#). However, contrary to altered visual temporal discrimination, auditory temporal discrimination and olfactory function have not been found to be statistically altered in LD patients, suggesting that these are likely not candidate endophenotypic markers of LD [\[179\]](#).

Obviously, sensory processing is often coupled with motor output. In daily life, perception and action are part of an interactive cycle, as we perceive the results of our action

through our senses, and sensory feedback are used to initiate or correct our movements. In task-specific FHD, conditions during which somatosensory and proprioceptive information is used to further plan the movement, elicited impaired activation of primary sensorimotor cortices, as well as posterior parietal and premotor areas [\[169\]](#). This importantly suggests that parieto-premotor dysfunction is also present during the delay when patients had to use somatosensory information for motor planning.

Nodal weighting

Because dystonia appears to involve larger networks than originally thought, investigating the relative weight of individual regions (nodes) in the functional and structural networks can provide a better understanding of the network's complex disorganization. Moreover, focusing on pathological models with dysfunction in a particular node could help answer the question of the node's contribution within the network. In this line of reasoning, a study considered two genetically modified mouse models of DYT1 dystonia, the first had conditional knock-in (KI) in neurons that express dopamine-2 receptors (D2-KI), while model 2 had conditional KI in Purkinje cells of the cerebellum (Pcp2-KI) [\[180\]](#). The results suggest that, in DYT1, dopaminergic D2 neurons have detrimental effect on sensory functions and functional connectivity, whereas the cerebellum functional role within the sensorimotor network protects against dystonia-like motor deficits. Cerebellar involvement in FHD depends on the complexity of symptoms, also suggesting a compensatory role of the cerebellum [\[160\]](#). Along the same line of reasoning, a rare form of dystonia with ADCY5 mutation presents a primary dysfunction within the striatum but not in the cerebellum [\[181\]](#). The ADCY5 pathological model provides the unique opportunity to test how a primary striatal dysfunction affects cerebellar activity, which we expect could compensate for striatal dysfunction. However, in the most common forms of dystonia, whether cerebellar abnormalities are primary or secondary to striatal dysfunction remains unclear. In a study involving patients with PRRT2 mutation, which induces dystonia among other hyperkinetic symptoms [\[182\]](#), aberrant cerebellar output can drive striatal dysfunction [\[72\]](#). In some cases, the cerebellum can have detrimental influence within the sensorimotor network such as in dystonic tremor [\[183\]](#), or in myoclonus dystonia (DYT11) [\[166, 184\]](#). Despite its systematic involvement in multiple forms of dystonia, the cerebellum likely has different functional weights within the sensorimotor network, depending on environmental and genetic factors.

Network analytics

Eidelberg et al. developed a method to map disease networks in rs-fMRI data based on independent component analysis (ICA) [\[185, 186\]](#). Applying this approach to scans from clinically manifesting (MAN) dystonia mutation carriers and healthy

control subjects, an rs-fMRI-based DytRP was identified (Figure 3A) with topographic features similar to its earlier PET counterpart [187]. As with the PET-based DytRP, expression of the rs-fMRI network was elevated in NM mutation carriers and in patients with sporadic dystonia (Figure 3B) and correlated with clinical dystonia ratings measured in affected individuals. This network mapping approach also allowed for detailed analysis of the functional connections linking DytRP nodes, as had been undertaken previously in Parkinson's disease [188, 189]. Genotypic and sporadic dystonias were both characterized by positive correlations between CbTC and pontine DytRP regions, suggesting distinct facilitatory nodal interactions in these groups. This contrasted with the negative correlations between CbTC nodes that were present in healthy subjects. Of note, increases in cortico-striatal or cortico-cortical connectivity were more pronounced in patients with genotypic forms of the disorder.

Recent studies of disease network architecture using graph metrics such as degree centrality, clustering, path length, and small worldness [187–190] identified differences in the patterns of functional connectivity in dystonia mutation carriers with and without motor manifestations. The data overall show how network mapping and graph theoretic methods can provide novel insights into the circuit abnormalities that underlie isolated dystonia. Other methods consider the inter-dependent involvement of cortical and cerebellar nodes, given the degree of convergence between cortical inputs on cerebellar nodes [191]. Such methods could bring more insight into the functional roles of the cerebello-cortical subdivisions in the pathophysiology of dystonia.

Summary of fMRI

The conclusions drawn from these resting-state and task-related studies converge towards 1) common networks that are affected in most forms of dystonia involve sensory cortices, striatum, and cerebellum; 2) cortico-cortical projections associated with abnormal representation of fine motor skills, i.e., parieto-premotor connections; and 3) network dysfunction extending to include cognitive-limbic associative nodes. Whether certain nodes have deleterious or beneficial contribution to behavioral output or clinical symptoms should be probed using specific pathological models and/or neuromodulation strategies [72] used in conjunction with fMRI.

Electroencephalography (EEG)

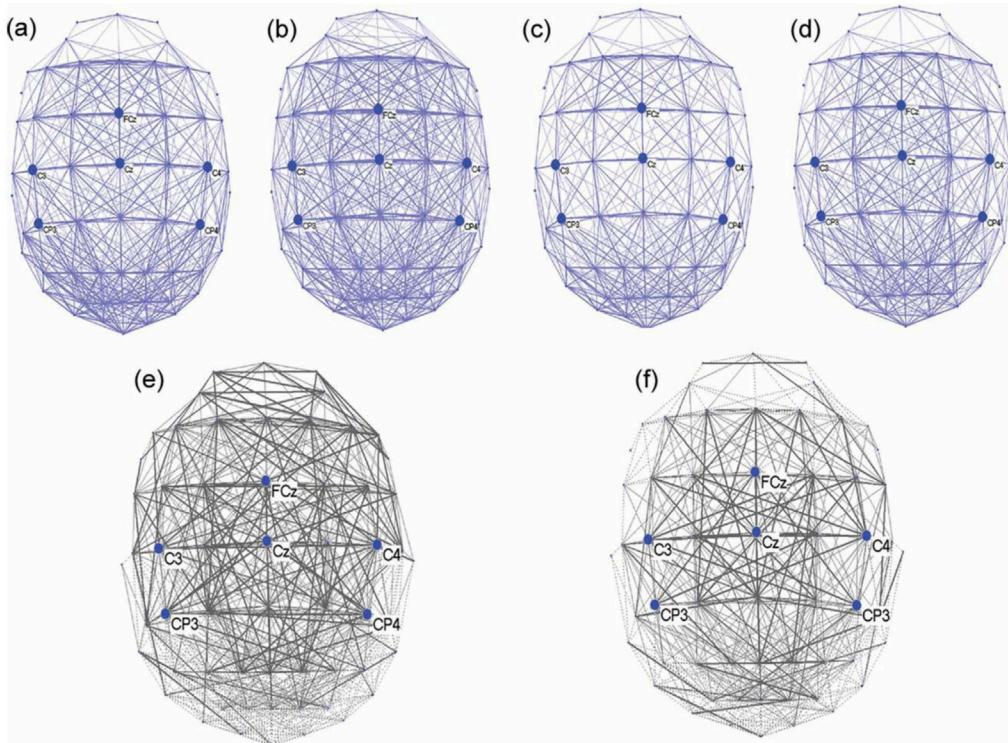
Although used in only a few studies of dystonia, EEG is one of the oldest non-invasive measures of brain function [4, 192] and allows comparisons of activity between groups at rest and during tasks. While scalp recordings generally reflect underlying cortical activity, source-modeling techniques enable deeper

localization. EEG signals can be decomposed into frequency bands since different frequencies reflect different brain processes. Thus, it is possible to get frequency information over time from various brain locations, largely limited to the cortex. Correlations between pairs of EEG channels can indicate communication between regions or indicate that both are jointly influenced from a third source. Correlations are referred to as functional connectivity. Using more sophisticated algorithms, it is possible to identify the causal influence of one region on another—this is called effective connectivity. The analysis of all (or many of) the possible connections in one model is called graph theory, and this gives a more systemic picture of the brain network.

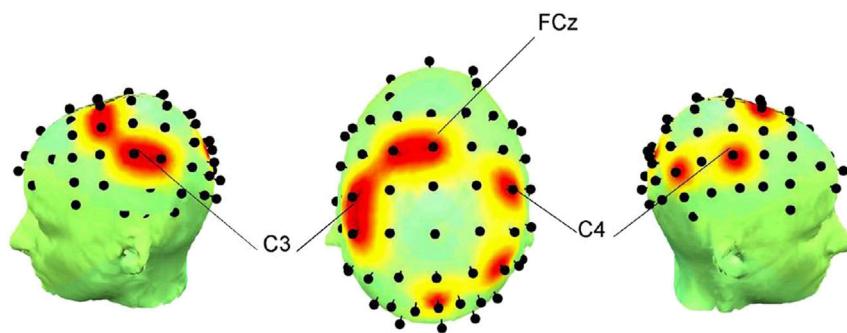
Most of the studies applying EEG to dystonia have been done in FHD. Somatosensory evoked potential studies show distorted digit representation in the somatosensory cortex [130, 193]. FHD patients also exhibit task-specific patterns in their EEG distinct from healthy controls [86]. Abnormal shape and amplitude of readiness potential were observed during motor preparation [194]. In the bilateral sensorimotor cortex, writing elicits increased low gamma power and less mu-beta and beta attenuation. There is also reduced connectivity between the SMA and the left sensorimotor cortex. During finger-tapping, patients failed to attenuate the mu-alpha, mu-beta, and beta power, and there were no changes in connectivity.

Brain connectivity in FHD compared with healthy controls was studied with 58-channel EEG using a technique called mutual information analysis [195]. Studies were done at rest and during a simple finger tapping task that did not produce dystonia. Mutual information is a measure of linear and non-linear coupling and was computed in alpha, beta, and gamma frequency bands. Most of the interest was linear and in the beta band. The task produced increased mutual information in both groups. However, mutual information was decreased in the patients at both rest and in action (see Figure 5). The data from healthy volunteers were then analyzed with graph theory using a measure of efficiency [196]. Efficiency during the finger tapping was increased selectively in the beta band, and regional efficiency was most increased in bilateral primary motor and left sensory area. A similar analysis was done in the FHD patients with different results [197]. While the beta network was efficient at rest, the efficiency decreased with the motor task (see Figure 6). Evaluating the regional efficiency, there was an increase over the SMA, but it decreased with the motor task. Collectively, the findings indicate an abnormal network at rest, greater disruption with a motor task, and motor area inefficiencies.

Several subsequent similar studies in FHD all used different methods. One study employed an isometric movement that did not induce dystonia, utilized magnetoencephalogram (MEG), and focused specifically on coherence between sources at M1 and S1 [198]. Coherence in different frequencies was similar at rest and was reduced only during movement in patients and only in the gamma band. A second study, again using non-symptomatic

**FIGURE 5**

EEG beta band functional connectivity in healthy volunteers in rest (a) and task (b) conditions and in FHD patients in rest (c) and task (d) conditions. Corresponding task-related changes in healthy volunteers (e) and FHD patients (f), with solid lines indicating increased connectivity during a task and dotted lines indicating decreased connectivity during a task. Six bold nodes are channels of interest. Reproduced with permission from [200].

**FIGURE 6**

Normalized spatial distributions of *Enodal*, a measure of global communication efficiency in beta band at each node, viewed from the left, top, and right aspects. Labelled channels exhibit significantly different *Enodal*, at a cost of 0.28 corresponding to the maximal interaction in *Eglob* differences. Main group effect found at FCz, corresponding to the SMA. Reproduced with permission from [202].

movements, used effective connectivity of EEG and machine learning [199]. The most sensitive difference between patients and healthy volunteers was a decrease in beta effective connectivity during movement from the contralateral

premotor area to other nodes. A third study using EEG coherence looked at writing, sharpening a pencil (a task that did not induce dystonia), and imagination of those same two tasks [200]. The only abnormality identified was a reduction of

interhemispheric alpha coherence between the two motor areas and only during actual handwriting. A fourth additional study used EEG transfer entropy at rest and during writing to evaluate effective connectivity [201]. They used graph analysis metrics and found reduced nodes in the beta frequency during writing. When investigating imaginary coherence during the processing of somatosensory information used to plan sequential finger movements, communication between parietal and frontal electrodes was decreased at mu and beta frequencies in writer's cramp compared to healthy controls [169].

In LD, symptomatic speaking was compared to two asymptomatic tasks—whispering and writing—using high-density EEG [202]. Speaking produced increased gamma synchronization in middle/superior frontal gyri, primary somatosensory cortex, and superior parietal lobule, with disrupted prefrontal–parietal coupling. Writing showed decreased beta synchronization, most prominently in right superior frontal gyrus; whispering was normal.

Despite methodological differences, results converge: focal dystonia shows sensorimotor-network disconnection—stronger during movement than rest—primarily affecting prefrontal–parietal links, with abnormalities variably in alpha, beta, or gamma bands. EEG/MEG therefore provide valuable spatiotemporal insight; combined with DBS they can probe cortical–subcortical coupling, and improved montages/ analytics may enable deeper source localization and open new horizons for investigating cerebello-cortical electrophysiological signals [203].

Deep brain stimulation (DBS)

For some types of dystonia—especially including but not limited to the generalized forms—DBS has been a revolutionary treatment. DBS also enables direct probing of dystonia networks. First, DBS activation, combined with imaging, can point to associated network changes. Effective DBS for dystonia—usually in the GPi—is associated with increased metabolism not only at the stimulation site but also in related network nodes of STN, putamen, and primary sensorimotor cortices [204]. GPi DBS also normalizes functional coupling patterns in the basal ganglia, thalamus, and brainstem [205]. Although less commonly used in dystonia, preliminary evidence suggests that STN and thalamic motor targets can show subtype-specific efficacy for PSP, CD, and appendicular forms of dystonia [206].

Second, DBS in unconventional targets can provide additional evidence about the regions and networks implicated in dystonia. DBS in the field of Forel in a small series of otherwise refractory dystonia cases, including one each of lingual, crano-cervico-axial, and hemidystonia, implicates the pallidothalamic tracts, i.e., the primary GPi output to thalamic nuclei [207]. Likewise, the pedunculopontine nucleus (PPN) has

been implicated in dystonia [208] and although not usually a DBS target for isolated dystonia, DBS in PPN can decrease the axial dystonia evident in Parkinson's disease [209].

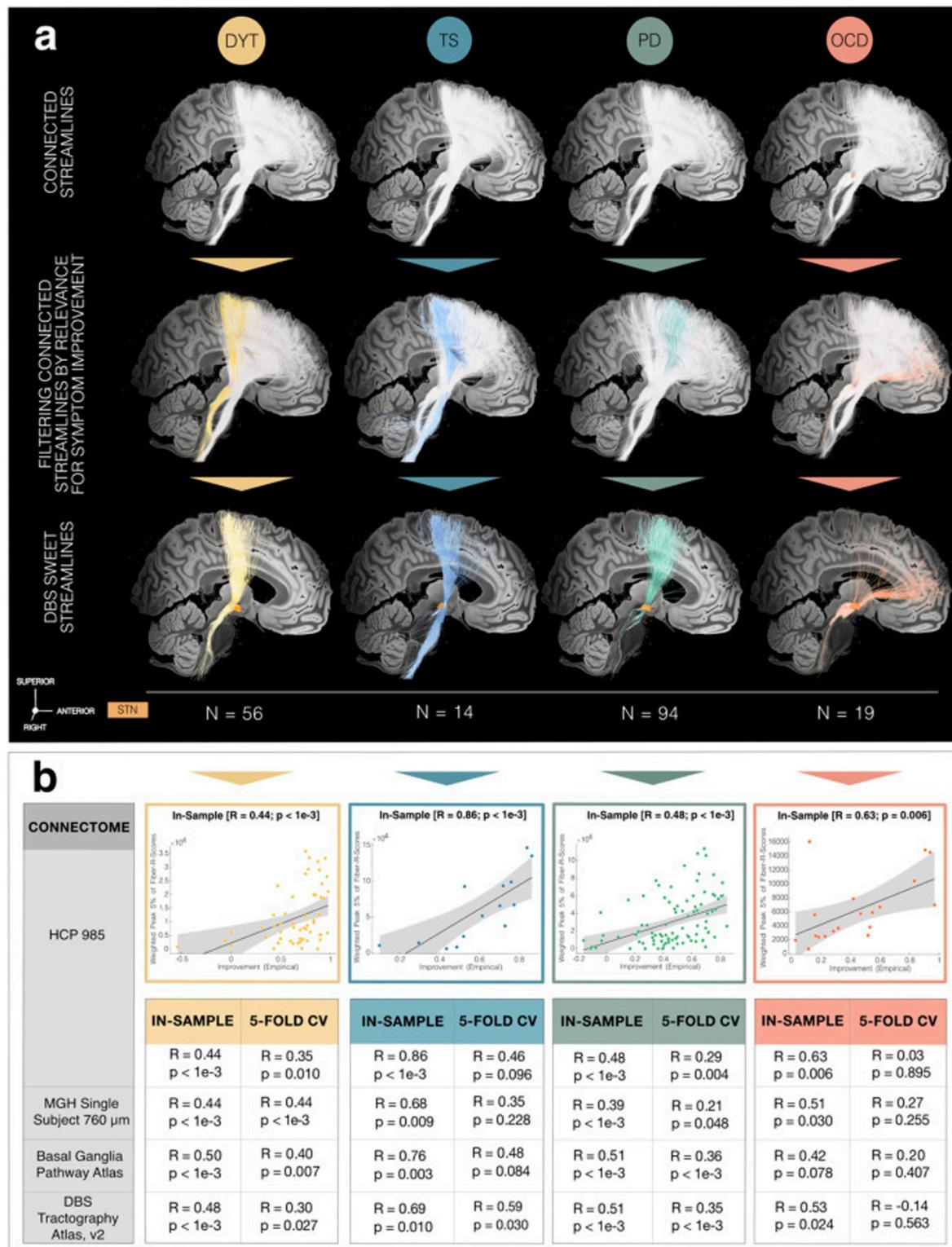
Third, and perhaps more significantly, the implantation of DBS electrodes for the treatment of dystonia provides an otherwise rare opportunity to understand network abnormalities through invasive brain recording in humans. Invasive human brain recording is evolving in several ways. Earlier work was based on brief recordings done intraoperatively or via leads externalized temporarily. The new availability of commercial DBS devices that provide brain sensing as well as stimulation, allows a shift to a chronic recording paradigm [210]. Paired with wearable monitors of motor function, chronic brain recording is ideal for a deeper understanding of personalized neural signatures of specific motor signs. The field of invasive recordings is also transitioning from single site recording (basal ganglia only) to multisite recordings, which can include other subcortical regions as well as sensory and motor cortex through insertion of electrocorticography leads through the same surgical exposure as the DBS leads.

DBS electrode localization and diffusion MRI

Co-registering DBS electrode locations to a standard stereotactic space can be a powerful method to explore several key questions [211]. First, signatures from electrophysiological recordings can be mapped to anatomical space. Elevated local field potential activity in the theta band recorded from GPi-DBS electrodes correlates with symptom severity in CD [212] and this localizes to the posterolateral GPi.

Although much of the data are from rodent and non-human primate models, evidence including recordings from DBS patients suggests multiple changes in GPi neuronal physiology: lower firing rates, firing patterns that are less tonic and more irregular and bursty, increased oscillatory power in delta (1–3 Hz) and theta (3–8 Hz) ranges, and broadened somatosensory receptive fields, especially for symptomatic body regions (as reviewed in a proposed box-and-arrow network model of dystonia pathophysiology [213]).

Second, electrode localizations could help identify an optimal stimulation site (“sweet spot”). A multi-center study of 87 patients linked best outcomes to stimulation sites in the posterolateral GPi and, more precisely, its ventral border [214]. While considering this location as an optimal spot, the distribution of optimal contacts across this large cohort varied widely, suggesting subtype, pathology, and somatotopic symptom expression were important predictors of optimal DBS response. In other words, there may not be one optimal DBS target for all patients with dystonia.

**FIGURE 7**

Sweet streamline models in the context of bilateral STN DBS implants. **(a)** Sweet streamlines ($n = 56$; peak $R = 0.36$) associated with beneficial stimulation outcomes were filtered from a population-based group connectome. The top row demonstrates the set of connections (in white) seeding from stimulation volumes across patients. Among these plain connections, only those were isolated via DBS Fiber Filtering (middle row) whose modulation was Spearman's rank correlated with clinical outcomes (bottom row). Sweet streamlines are displayed in thresholded and

(Continued)

FIGURE 7 (Continued)

binarized fashion. Results are shown against a sagittal slice ($x = -5$ mm) of the 7T MRI *ex vivo* 100- μ m human brain template, in conjunction with a three-dimensional model of the right STN in template space from the DISTAL atlas, version 1.1. (b) In-sample correlations and 5-fold cross validations are reported for models informed on normative connectomes. Plots in the top row represent the fitting of a linear model to determine the degree to which the overlap of E-field magnitudes with selected HCP 985 Connectome sweet streamlines explains variance in empirical clinical outcome across the cohort, as calculated using Spearman's correlation (two-sided tests). The magnitude of E-field overlap with sweet streamline models in this analysis is expressed as weighted peak 5% of Fiber R scores under each E-field, averaged across bilateral scores per patient. Gray shaded areas indicate 95% confidence intervals. Reproduced with permission from [5].

Third, electrode localizations could also link treatment outcomes to distributed brain networks. In the past and in other diseases, tractography derived from dMRI has been used to associate DBS stimulation sites with structural brain networks [215–219]. However, tractography in the pallidal region is problematic because of its proximity to the internal capsule. Cortical input to the pallidum is known to traverse mainly through the striatopallidofugal bundle [220]. However, when seeding connections from the pallidum using dMRI based tractography, many results include the internal capsule as a false positive connection [221]. A potential solution to this problem was introduced by a basal ganglia atlas that had not been constructed based on tractography but on expert anatomical knowledge [222]. Pathways included in this resource should be free from false-positive connections, and all included tracts will match our current anatomical knowledge.

This detailed atlas was applied to DBS electrode localizations in 80 patients from five institutions to study networks associated with optimal response in cervical and generalized dystonia [223]. While this study confirmed that optimal stimulation sites mapped to the posterolateral somatomotor region of the GPi, it provided evidence for differential treatment mechanisms in cervical vs. generalized dystonia. Namely, response in CD mapped to pallidofugal fibers that projected radially into the internal capsule, along the main axis of the basal ganglia, such as the comb system of Edinger [224]. In contrast, optimal response in generalized dystonia mapped to pallidothalamic bundles such as the ansa and lenticular fasciculi. While projections of both systems are known to reunite in the thalamus, the finding could motivate differences in networks associated with cervical and generalized forms of dystonia. This overall approach of using DBS treatment outcomes to make inferences about networks implicated in dystonia has also been extended to STN-DBS (see Figure 7) [5]. Recently, a larger study was carried out to elucidate optimal stimulation sites and networks in subthalamic DBS for dystonia [206]. While axial forms of dystonia (such as cervical and truncal phenotypes) were best treated by directing the electrical field to the ventral oral posterior nucleus of the thalamus (and cerebellothalamic circuitries), appendicular forms were best treated when stimulating the subthalamic nucleus proper (and basal ganglia circuitries).

In sum, these three examples show the unique potential and insights gained from studies that combine precise DBS electrode reconstructions with tractography from dMRI and can compare

electrophysiology, clinical effects and involved networks on a group level [225].

Simultaneous recordings in GPi and thalamus in pediatric movement disorders

Dystonia is a prominent symptom of many pediatric movement disorders. To refine DBS targeting in pediatric movement disorders with heterogeneous distributions of CNS pathology, a protocol was developed using temporary depth electrodes at multiple candidate sites. Recording and test stimulation are performed over 5 days in a neuromodulation monitoring unit (NMU) with the child awake and able to participate in usual daily activities [226]. Subsequently, a total of four permanent DBS leads are implanted, usually in a combination of pallidal and thalamic targets [226]. This procedure raised the success rate in children with secondary dystonia from 50% to greater than 90%, and it expands the potentially effective targets. Diagnoses include secondary dystonia, primary dystonia, and Tourette syndrome. Only one of the 33 children did not proceed to permanent electrode implantation due to lack of an effective target [227].

These recordings yield new insight into DBS mechanisms for dystonia and related movement disorders. Stimulation-evoked potentials captured simultaneously across depth electrodes at multiple DBS frequencies reveal inter-regional connectivity and the spatiotemporal spread of stimulation. Comparison of correlations in spontaneous brain activity with the evoked potential shapes suggests that the DBS signal propagates at least partly along physiological pathways, enabling frequency-dependent maps of orthodromic and antidromic propagation useful for parameter selection.

Clinical results up to 5 years after implantation in children with secondary dystonia suggest that stimulation in the optimal thalamic target can almost completely alleviate the hyperkinetic component dystonia, whereas stimulation in the optimal target in GPi only partly alleviates the hypertonic component. This observation suggests that the mechanism of the hyperkinetic and hypertonic components may be different, and support symptom-specific target selection in pediatric cases.

Unexpectedly, both GPi and thalamic regions are relatively quiet at rest and increase their activity with attempts at voluntary movement [226, 227]—opposite the typically high resting GPi

activity in Parkinson's disease and in healthy non-human primates. Because GPi outputs inhibit thalamic targets, an excitatory drive to thalamic targets has been suggested, most likely arising from cortical glutamatergic efferent pathways back to thalamus. This supports a model in which the basal ganglia normally modulate and select activity in thalamocortical loops, and decreased firing in GPi leads to failure of modulation and selectivity. This could provide an explanation for both hypertonia due to excessive drive to motor cortices, as well as hyperkinetic movements due to failure of inhibition of unwanted thalamocortical dynamics. Further studies are needed to determine the mechanism by which stimulation in GPi or thalamus can selectively ameliorate these different components of dystonia.

The specific network functions of thalamic relays between cerebellum and striatum [228, 229], and indeed even different thalamic motor nuclei (i.e., Voa/Vop and VIM), still need to be elucidated and may play an important role in dystonia. In two adolescents with dystonia secondary to cerebral palsy, compared to a Tourette patient without dystonia, there was a drawing task-related increase in magnitude of activity in the GPi and Vim nucleus of the thalamus [230]. There was no such difference in other thalamic nuclei. Because GPi and Vim are the primary nodes in BG and cerebellar output pathways, respectively, it implicates both pathways in the altered motor control evident in this form of dystonia. A follow-on study supported the higher activity in the GPi, as well as stronger coupling from STN to GPi than from GPi to STN [231].

In pediatric dystonia, benzodiazepines reduce BG and thalamus activity and the efficacy of transmission between them [232], so future studies also need to carefully control for the influence of oral medications.

Oscillopathies

The theoretical foundation for network models of movement disorders—including Parkinson's disease as well as dystonia—now incorporates an “oscillatory synchronization” framework, the idea that abnormal synchronization of neuronal populations underlies specific signs and symptoms across brain disorders. One emerging concept is that the extent to which DBS attenuates pathological synchrony serves as a key biomarker of therapeutic efficacy [23, 233–235]. This principle, established in modeling motor fluctuations in Parkinson's disease [236], is now being applied to dystonia.

Local field potentials and electrocorticography provide sensitive measures of oscillatory synchronization (see EEG section). Theta band (4–8 Hz) oscillatory activity within motor networks of the basal ganglia and cortex is associated with adult-onset CD [212]. Recently identified cortical gamma band oscillations (60–80 Hz) may represent another signature of dystonia [237]. Characterizing these rhythms is directly

informing therapy, enabling identification of stimulation paradigms and parameters that normalize exaggerated oscillatory patterns. Current sense-and-stimulate devices could support even richer network analyses if they allowed recording with higher channel counts and could be attached to a wider variety of leads tailored for different recording sites.

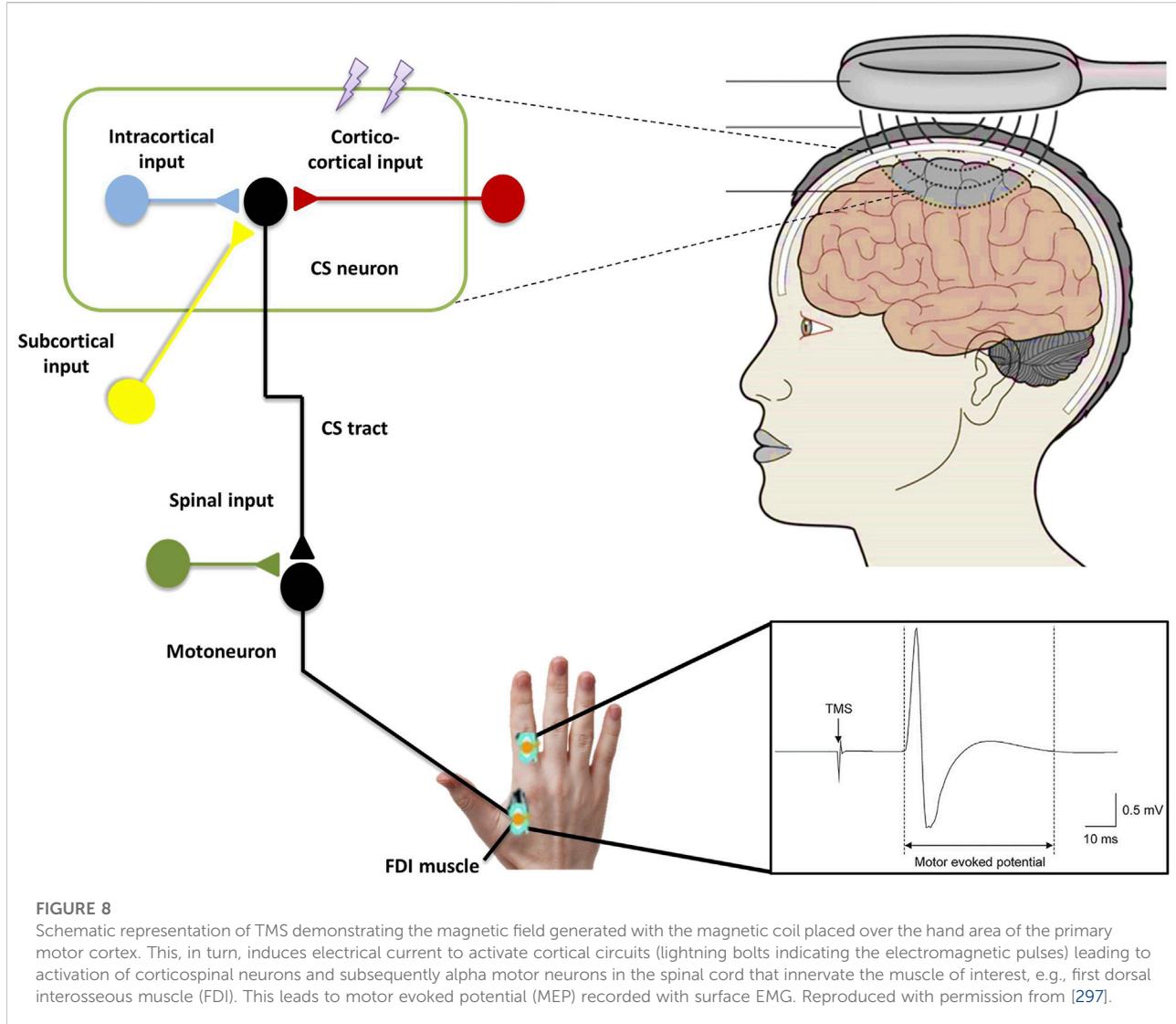
Non-invasive brain stimulation (NIBS)

The vast majority of dystonia patients do not undergo DBS surgery. Non-invasive brain stimulation (NIBS) methods provide less direct but still meaningful ways to modulate neural activity. Although generally limited to targeting only superficial structures like the cortex, NIBS can influence wider interconnected networks, including deeper structures, as demonstrated by combined neurophysiological and imaging studies showing widespread changes [238, 239].

Because dystonia pathophysiology involves decreased inhibition across multiple levels of the nervous system leading to co-contraction of agonist and antagonist muscles, distorted digit representation associated with loss of surround inhibition, and possibly excessive plasticity, most NIBS studies have aimed to reduce cortical excitability, which has been hypothesized to lead to increased inhibition and reduced abnormal plasticity. Accordingly, prior work has used rTMS or low-intensity TES such as tDCS to target nodes in the dystonia network, such as the motor cortex, premotor cortex, SMA, or cerebellum.

Transcranial magnetic stimulation (TMS)

Many studies in focal dystonia have used transcranial magnetic stimulation (TMS), the most widely used form of non-invasive brain stimulation. It can be applied with many different protocols, the simplest involving motor cortex stimulation and measurement of corresponding muscle activation (see Figure 8). Repetitive TMS (rTMS) is commonly used to induce plasticity. Most rTMS studies in dystonia employ designed inhibitory protocols such as low frequency (~1 Hz) rTMS [17] or continuous theta burst stimulation (cTBS) [240]. FHD is the most studied condition. Low frequency rTMS over the primary motor cortex [241] and premotor cortex [242, 243] improves writing in patients with FHD. In CD, one study testing several cortical sites found that a single session of 0.2 Hz rTMS to dorsal premotor cortex and motor cortex stimulation produced the greatest reduction in dystonia [244], while 10 sessions of bilateral cerebellar cTBS reduced CD severity relative to sham stimulation [245]. In FHD and CD, a single session of repetitive cerebellar stimulation produced distinct immediate post-effects on cortical plasticity: cerebellar regulation of cortical plasticity was lost in FHD, but preserved in CD [246]. In CD, neck proprioceptive inputs may modulate the relationship between

**FIGURE 8**

Schematic representation of TMS demonstrating the magnetic field generated with the magnetic coil placed over the hand area of the primary motor cortex. This, in turn, induces electrical current to activate cortical circuits (lightning bolts indicating the electromagnetic pulses) leading to activation of corticospinal neurons and subsequently alpha motor neurons in the spinal cord that innervate the muscle of interest, e.g., first dorsal interosseous muscle (FDI). This leads to motor evoked potential (MEP) recorded with surface EMG. Reproduced with permission from [297].

cerebellar output and cortical plasticity [246]. In FHD, loss of cerebellar control over sensorimotor plasticity correlated with impaired adaptive reaching [247]. In BSP, low frequency rTMS to the anterior cingulate cortex has yielded promising results [248]. In summary, inhibitory rTMS targeting premotor cortex, motor cortex, and cerebellum appear potentially beneficial for FHD and CD, whereas the anterior cingulate cortex is a promising target for BSP. Larger randomized controlled trials are still needed.

Future TMS studies in dystonia should control for pharmacologic state. In a study of FTSD with 24 participants, Zolpidem flattened rest and active input/output curves and reduced ICF compared to placebo [92]. BoNT also influences central physiology and therefore the response to TMS. In general, BoNT decreases sensorimotor activation during voluntary movements [249]. Electrophysiological evidence from TMS and reflex studies suggests BoNT-related plasticity in cortex and brainstem, respectively [250]. These plastic changes may persist, as

clinical observations indicate lasting modifications of dystonic motor features beyond individual BoNT cycles.

FHD is also associated with plasticity—as measured using TMS in with a paradigm known as paired associative stimulation—that is excessive [251, 252], and abnormally regulated [253]. However, the findings remain controversial because some studies did not find excessive plasticity in dystonia [254]. Nevertheless, the complex longitudinal dynamics of various types of plasticity in dystonia, and the ability of TMS to measure and modulate plasticity at a macroscopic level, make plasticity an important direction for future research with TMS.

Transcranial electrical stimulation (TES)

TES encompasses both tDCS and tACS. A study using cortical cathodal (excitatory) tDCS over motor cortex found

no benefit in FHD [255], whereas anodal tDCS of the ipsilateral cerebellum produced conflicting results [254, 256]. In musician's dystonia, improvements have been reported with cathodal tDCS to the motor cortex of the affected side and anodal tDCS to the unaffected side combined with motor training [257] or with bilateral parietal (cathode left, anode right) tDCS [258]. Although no formal studies exist in CD, case reports describe benefit from bilateral anodal cerebellar tDCS [259] and bilateral motor cortical 15 Hz tACS [260]. Overall, evidence for tDCS or tACS in dystonia remains preliminary, and further studies across different subtypes are needed.

Transcranial ultrasound stimulation (TUS)

Low-intensity TUS is a novel NIBS method offering greater focality and penetration depth than other NIBS modalities. This is particularly important for dystonia, as several of the regions implicated are deeper, subcortical structures. Human studies show stimulation duration-dependent reductions in cortical excitability during the application of TUS (the “online” effect) [261]. Plasticity or offline effects have also been demonstrated. In non-human primates, fMRI demonstrated that 40 s of TUS to the frontal polar cortex or SMA altered functional connectivity between each site and their normal “connectional fingerprint” – the cortical areas with which they normally show connectivity as determined by BOLD correlations, e.g., for SMA it is primarily M1, superior parietal lobe, and middle cingulate cortex—for up to 60 min [262]. In humans, 80 s of TUS delivered in a theta burst pattern increased cortical excitability for at least 30 min [263]. In Parkinson disease and dystonia, recordings from DBS electrodes in the GPi showed that TUS can effectively modulate GPi activity, producing protocol-specific changes in neural activity [264]. Collectively, these findings position TUS as a promising non-invasive neuromodulation approach for dystonia.

Integrating brain imaging and NIBS: toward multimodal, personalized noninvasive neuromodulation

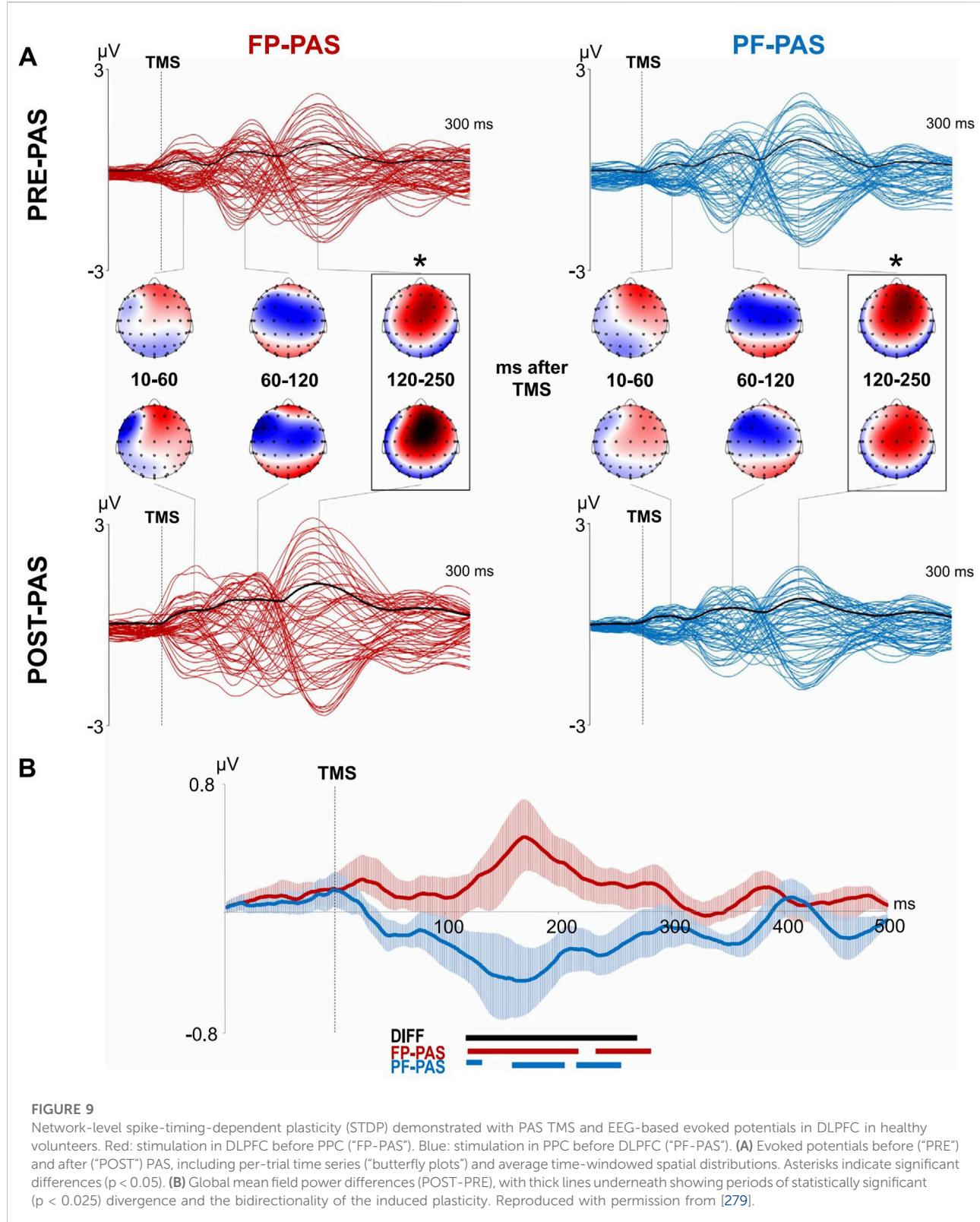
Dystonia is a multifaceted condition; therefore, multimodal approaches that integrate neuroimaging and neurophysiology data into a unified pathophysiological framework offer a logical path toward deeper understanding and improved treatment. Within this context, NIBS techniques provide valuable tools for probing brain activity, elucidating mechanisms, and identifying novel therapeutic targets. In particular, TMS and TES can be combined with electrophysiology or neuroimaging to determine: 1) *where* to stimulate, by tailoring target regions to each patient's individual anatomy or functional fingerprint; 2) *how* to personalize stimulation parameters (e.g., intensity,

frequency) based on individual connectomic and biophysical models using structural and fMRI data, and 3) *when* to deliver stimulation by employing closed-loop, feedback-triggered paradigms guided by online measures such as EEG.

The optimal neuroimaging technique depends on the intervention's objective. Structural MRI (T1- or T2-weighted) is highly effective for anatomical targeting, but combining it with metabolic (e.g., PET) and functional modalities (e.g., fMRI, ASL) has become standard practice for target selection [265]. Recent advances in hardware now enable modulation of neural *circuits* rather than isolated cortical areas, allowing simultaneous engagement of multiple network nodes and even interaction between networks [266]. This can be accomplished, for instance, with multicoil TMS, including cortico-cortical paired-associative-stimulation paradigms that deliver semi-synchronous stimulation to two brain regions [267]. Because this approach relies on Hebbian spike-timing-dependent plasticity, tuning it to circuit timing—by integrating diffusion imaging [268] and EEG—should permit measurement and modulation of network-level dynamics relevant to dystonia pathophysiology. Similarly, multichannel TES montages can focally stimulate specific cortical targets and simultaneously stimulate different areas belonging to the same or different networks to probe their dynamic interplay [269]. Recently developed biophysical modeling algorithms derive features from individual neuroimaging data to create realistic 3D head models and simulate stimulation-induced electric field distributions induced by TES or TMS [270, 271]. Such personalized models not only improve field control but also allow optimization of stimulation parameters in advance, enhancing precision and efficacy.

Multimodal NIBS can also be delivered online by combining TES or TMS with neurophysiology recordings such as scalp EEG. Simultaneous TMS-EEG paradigms allow measurement of the brain's real-time response to direct perturbation, enabling study of causal interactions between regions with high temporal resolution and providing insight into effective connectivity, cortical inhibition/excitation, and plasticity [272]. Macroscopic, network level forms of spike-timing dependent plasticity can be induced using two-site TMS and the effects quantified with evoked potentials in the EEG (see Figure 9) [273]. The combination of TES-EEG methods can increase the temporal precision of TES manipulations and enable brain state-dependent modulation. In closed-loop tACS-EEG protocols, phase and amplitude of ongoing brain activity are used to automatically adjust stimulation parameters and maximize entrainment of neural activity. This approach has been used, for example, to enhance slow-wave sleep and memory consolidation [274, 275] and could be adapted to target pathological oscillations in dystonia in real-time.

In summary, NIBS paradigms benefit substantially from integration with imaging methods, providing extensive information about cortical functional dynamics with high



temporal (e.g., EEG) and spatial (e.g., MRI) resolution. However, a comprehensive review of NIBS studies across different dystonia subtypes [276] concludes that the results to date remain inconclusive. A likely reason is that most studies have targeted only a single stimulation site—typically somatosensory cortex, primary motor cortex, dorsal premotor cortex, or cerebellum [9, 277] – rather than addressing network-level dysfunction. Supporting this view, a recent study demonstrated top-down causal alterations of functional connectivity within the sensorimotor network in isolated focal dystonia [135]. Future work should therefore prioritize personalized multimodal stimulation protocols designed to influence both within-network and between-network dynamics.

Computational models

The brainstem and the neural integrator model

A key motivation for considering brainstem dysfunction in dystonia came from elegant clinical observations of head movements in CD [278]. In some patients, rotating the head away from the clinical null position toward a desired target is followed by an involuntary slow drift back towards the null, then a faster corrective movement toward the target. This pattern resembles gaze evoked nystagmus, which occurs when cerebellar feedback to the oculomotor neural integrator is impaired [279]. This prompted the question of whether an analogous neural integrator exists for head movements and whether it is dysfunctional in CD. Experimental work in animals points to a midbrain region—the interstitial nucleus of Cajal (INC) – as having properties consistent with a head-movement neural integrator [280]. This hypothesis is compelling for two reasons. First, it shifts attention to the brainstem, where inputs from a range of neuroanatomical locations and sensory modalities converge on the neural integrator. The neural integrator hypothesis can, therefore, accommodate the considerable diversity of findings in the literature; malfunction in any one of the inputs or the integrator itself could result in the abnormal neural control of head movements. Second, it yields testable predictions; for example, cerebellar and proprioceptive inputs to the INC become potential targets for central or peripheral neuromodulation.

Beyond the neural integrator model and the INC, three additional points about the brainstem are noteworthy: 1) although most of INC's connections are with brainstem, spinal cord, and cerebellar regions, the PPN is another key integrative brainstem nucleus with reciprocal connections to BG and thalamus, providing a more direct interaction with BGTC loops heavily implicated in dystonia, 2) a theoretical framework based on rodent work implicates descending projections from basal ganglia to brainstem circuits in BSP [111], and 3) brainstem nuclei are seldom mentioned in lists of brain regions involved

in dystonia networks, likely because they are difficult to delineate in standard neuroimaging. Higher field strength MRI should begin to address this limitation. Future dystonia network models should therefore incorporate these and other brainstem nodes.

The virtual brain

Because dystonia seems to involve complex brain networks involving many regions, a potentially fruitful way to integrate and better understand pathophysiological data from many modalities is with computational simulations of those networks. For example, neuroimaging data can be merged with dynamic mean-field models to create large-scale brain simulations using a neuroinformatics platform such as The Virtual Brain (TVB; [281]). It is open source, written in Python, and includes a graphical interface to support usability. TVB is model agnostic: users can select from a library of mean-field models, ranging from simple oscillators to more complicated neural population models. In addition, the open-source framework allows users to add their own hypothesized model. Outside of dystonia, several applications of TVB have been demonstrated. Although recently adapted for mouse studies [282], TVB is most commonly used to model empirical human data (e.g., fMRI or EEG), to demonstrate how structural connectivity and local dynamics jointly shape intrinsic, resting state activity [283]. Initial clinical applications focused on stroke, where patient-specific models showed that local excitability predicted physiotherapy-related motor recovery. In epilepsy, development of the Epileptor model [284] enabled prediction of seizure focus location and is now being tested in a national clinical trial for clinical-decision support [285]. TVB has also been applied to dementia, where model parameters outperformed standard neuroimaging metrics in predicting cognitive performance across the disease spectrum [286]. More directly relevant to dystonia, recent work integrated detailed models of the basal ganglia in TVB to simulate DBS effects [287], demonstrating renormalization of circuit dynamics after stimulation and illustrating the potential to personalize stimulation parameters and target selection. TVB therefore represents a promising computational tool for investigating and treating pathophysiological brain networks in dystonia. Regardless of the specific modeling framework, the close coordination of modeling and experiments would inform each other in an iterative loop that facilitates progress in how we come to understand brain network pathophysiology in dystonia.

Discussion

Future imaging studies

Future dystonia research with all the imaging modalities should heed lessons learned from meta-analyses, which

commonly include a critical review of methodological details in past studies and make corresponding recommendations for maximizing the informativeness of future imaging experiments [40]. Relatedly, future imaging studies would also benefit from larger-sized cohorts and adopting ongoing advances in analytics. As in neuroscience more broadly, research into dystonia network pathophysiology should incorporate algorithmic advances from the broader field of network science [288]. As but one example, functional connectivity gleaned from rs-fMRI can benefit from widely used [135] and emerging [289] methods to infer causality in the networks. Yet, attention to rigor in quality control plays a critical role for interpretation of findings [84] and improved consistency would enhance reproducibility and facilitate meta-analyses.

Advances in DBS

When there is clinical justification to do so, DBS-associated recordings should take advantage of multiple recording sites, ideally simultaneously. In parallel, advances in DBS technology—whether via adaptive programming, coordinated reset stimulation protocols, or, ultimately, greater cell and circuit specificity—may provide not only greater treatment efficacy but also entirely new insights into the network pathophysiology of dystonia [23].

Vagus nerve stimulation (VNS)

VNS using an implantable device is an approved treatment for drug-resistant epilepsy and depression. When paired with rehabilitation, VNS improves upper limb motor function after ischemic stroke [290]. The vagus nerve can also be stimulated non-invasively via the outer ear, which receives cutaneous supply by the auricular branch of the nerve [291], or percutaneously in the neck—a method that has shown promise for treating freezing of gait in Parkinson’s disease [292]. Given these findings, and the vagus nerve’s indirect influence on prefrontal cortical and cerebellar regions through other brainstem nuclei, VNS—possibly combined with rehabilitation—may represent a potential therapy for dystonia.

Longitudinal dynamics

Most studies of network pathophysiology in dystonia are either cross-sectional or represent a small number of points in time (e.g., pre-/post-treatment). Although it would add an additional dimension to an already complex enterprise, evaluating how the network pathophysiology changes over longer time scales would strengthen understanding of the natural history of the disorder. If we had a better

understanding of this process, it could provide a foundation for developing disease-modifying therapies. As an important subset of this, developmental aspects of dystonias, especially for but not limited to childhood-onset dystonias, would benefit from investigations into how the brain networks implicated in dystonia develop [293].

Network implications of over-trained motor patterns

Our understanding of dystonia at the molecular level has expanded considerably over the past two decades [294]. Yet many dystonia subtypes, particularly focal forms, are also likely shaped by environmental influences [295, 296]. Task-specific dystonias, for example, have been linked to multiple environmental risk factors [297], and such features can help infer why motor control and skill reproduction break down under certain conditions [134, 298]. A motor-control framework is valuable not only because it clarifies mechanism, but also because it provides a shared language for discussing impairments with patients and for developing targeted interventions. One such intervention stems from the observation that patients appear trapped in an over-trained dystonic motor pattern and behavioral interventions that stochastically inject variability into movement repetitions during retraining can disrupt this pattern [299]. A substantial proportion of patients have returned to professional performance after such an intervention [300]. The neuroanatomical network underlying task-specific dystonia likely spans a broad sensorimotor hierarchy and will vary depending on whether one is trying to find the network responsible for vulnerabilities endowed by certain risk factors, the dystonia motor pattern itself, or the clinical trajectory of the disorder. That said, associative higher-order regions such as the premotor and parietal cortex emerge repeatedly across multiple research approaches [136, 298]. This task-specificity has motivated proposals for therapeutic brain-computer interfaces (BCIs) that enable patients to modulate pathological brain activity so that it more closely resembles activity during an asymptomatic task, with the expectation of symptom reduction [22]. A clinical trial of such a BCI intervention in LD patients (NCT04421365) is currently underway.

Can we target the dystonia network through a common dystonic phenotype?

As molecular insights expand, it is worth asking whether we have neglected the features of the dystonic phenotype itself [301]. Can dystonia as a phenotype—defined by its characteristic motor features rather than by etiology (e.g., DYT-TOR1A) or subtype

(e.g., adult-onset focal dystonia) – be investigated as a meaningful entity in its own right? The dystonic phenotype has reliable clinical features, recognizable kinematic characteristics, and many effective interventions act at the systems control level rather than the molecular level. For example, DBS provides substantial benefit in dystonia, yet its mechanism is comparatively coarse, most likely modulating activity or excitability of target regions rather than injecting normal patterns of neural activity or selectively modifying abnormal patterns [302]. This raises the question of whether shared kinematic signatures could help characterize dysfunctional networks in dystonia, analogous to how oscillatory movement features serve as teaching signals for adaptive neuromodulation of tremor [303, 304]. Likewise, neuro-physiotherapy engages the dystonic network in its entirety, and an emerging evidence base supporting its use for specific motor control axes within specific subsets of dystonia [305, 306]. Until targeted molecular therapies are available, approaches that act on common features of the dystonic phenotype may represent an effective way to both probe and modulate the underlying network.

Tremor and dystonia

Tremor is recognized as an important aspect of dystonia [6, 307]. Because of increasing interest in tremor in dystonia, and because the associated terminology continues to evolve, we consider this an important topic for future research into the network pathophysiology of dystonia. The term “dystonic tremor” has been widely used [308, 309], but the consensus from a group of specialists in dystonia and tremor have suggested that this term has had variable interpretations and can be misleading [310]. They suggest that the term “tremor” should be reserved for movements that are rhythmic, and that, in the context of dystonia, repetitive movements that appear grossly arrhythmic should be called “jerky dystonia.” But precisely how rhythmicity is operationally defined remains unclear. In our present treatment, our descriptions of dystonia with tremor include the traditional, broadly defined dystonic tremor.

In general, dystonia with and without tremor share the same overall circuit pathophysiology, encompassing basal ganglia, cerebellum, and sensorimotor cortex [311]. However, dystonia with tremor seems to exhibit a stronger contribution from CbTC loops that might be more rhythmically engaged. In dystonia with tremor in the upper limb or head, there was increased volume of motor cortex and the same thalamic region that shows tremor-locked activity, and cerebellum-thalamic connectivity was positively correlated with tremor power [183]. In the context of LD, dystonic voice tremor patients exhibited additional abnormalities on fMRI in medial frontal gyrus, cerebellum, and posterior limb of internal capsule [312]. Compared to

essential tremor, dystonic tremor patients exhibited greater reductions in functional connectivity between cortex, BG, thalamus, and cerebellum [161]. Single unit neuronal recordings during procedures previously used to ablate the INC for CD found firing properties that differed for CD with versus without tremor, for thalamic subregions receiving projections from either GPi or cerebellum [313]. The firing patterns in GPi may be more nuanced: CD with and without jerky tremor had similar firing patterns, but CD with sinusoidal tremor showed a different distribution of firing pattern properties [314, 315]. Interestingly, one study suggests that different types of tremor show different responses to non-invasive stimulation; tACS suppressed or enhanced tremor in a phase-dependent fashion for sinusoidal but not for jerky tremor, and for cerebellar but not motor cortical stimulation [316]. Collectively, the evidence to date suggests that networks involving the cerebellum play an important role in at least some types of tremor seen in dystonia.

Functional dystonia

Although this review was inherently focused on organic dystonia, contemporary views of functional movement disorders, including functional dystonia, view it as having pathophysiology that can inform our understanding of dystonia more broadly defined. Organic and functional dystonias exhibit substantial overlap in their brain network abnormalities, including decreased cortical inhibition [317, 318]. But there are also several differences. Functional dystonia exhibited decreased volume of caudate, nucleus accumbens, putamen, and thalamus [319]. At rest, functional dystonia’s metabolic demands measured with PET were increased in the cerebellum and BG and decreased in motor cortex, a pattern opposite of that found in organic dystonia [320]. Functional dystonia also exhibited decreased functional connectivity between the right temporoparietal junction and a) bilateral sensorimotor cortex [321] and b) dorsal and rostral prefrontal cortex [322]. Given the role of the temporoparietal junction in comparing internal predictions of motor intentions with actual motor events, this might explain the altered sense of self-agency characteristic of functional dystonia. Functional dystonia also may be associated with altered emotional processing, because during emotional processing tasks functional dystonia patients exhibited decreased activation in right medial temporal gyrus, bilateral precuneus, and left insula [323]. A limited number of cases of functional dystonia patients receiving DBS showed GPi firing rates similar to organic dystonia [324]. Non-invasive brain stimulation over left dorsolateral prefrontal cortex alleviated symptoms in functional dystonia, including intermittent theta burst TMS

[325] and anodal tDCS [326]. As with most research with organic dystonia, the study results are associations, and therefore cannot inform what is cause vs. effect in terms of brain network changes.

Summary

In summary, there is a large and growing body of evidence that has begun to characterize dysfunctional networks in dystonia. The evidence comes from a multitude of modalities for measuring brain regional and network activity in humans. Across the vast literature on this topic, it is difficult to determine how much specific dystonia subtypes, tasks, and study designs variously contribute to the heterogeneity of results [22]. In general, there is convergent evidence implicating networks that include primary sensorimotor cortical areas, several nuclei in the BG, the thalamus, the cerebellum, and the brainstem. However, there is also evidence for numerous additional regions, primarily in the form of a variety of cortical areas beyond primary sensorimotor territories, such as premotor, supplementary motor, and parietal cortices.

There is a synergistic relationship between the research into these networks and the development of new and improved treatments. Naturally, the research into the networks informs new treatment development. But also measuring brain network activity in response to treatment, as well as during the process of implanting DBS electrodes, for example, can inform understanding of the dysfunctional networks. Ultimately, as our knowledge of the specific dysfunctions of the intricate networks involved in dystonia improves, it should, in turn, give rise to improved and personalized therapies, including oral drugs, BoNT, DBS, and NIBS.

Author contributions

DP, MH, and KS conceived of the review concept and scope. DP, RC, DE, CG, AH, SL, AM, JP, AS, TS, ES, PS, JT, MH, KS contributed to the first draft of the manuscript. DP, MH, KS, TS, and CG conceived of and organized the figures. DP, MK, RC, DE, CG, AH, SL, AM, JP, AS, TS, PS, JT, MH, and KS edited and revised sections of the manuscript. All authors contributed to the article and approved the submitted version.

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In memoriam

This work is dedicated to the memory of Dr. Mark Hallett, a remarkable leader and generous mentor whose instrumental role in much of the research reviewed here continue to inspire and elevate our community.

Conflict of interest

CG and KS are members of the Dystonia Editorial Board upon submission of the manuscript. JT and MH(†) are members of the Dystonia Advisory Board upon submission of the manuscript. These memberships had no impact on the peer review process and the final decision.

The remaining author(s) declared that this work was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

Generative AI statement

The author(s) declared that generative AI was not used in the creation of this manuscript.

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Glossary

ACh	Acetylcholine	STN	subthalamic nucleus
ADSD	adductor spasmotic dysphonia	tACS	transcranial alternating current stimulation
AES-SDM	anisotropic effect size-based signed differential mapping	tDCS	transcranial direct current stimulation
BG	basal ganglia	TES	transcranial electrical stimulation
BGTC	basal ganglia thalamocortical	TMS	transcranial magnetic stimulation
BOLD	blood oxygen level-dependent	TUS	transcranial ultrasound
BoNT	botulinum neurotoxin	TVB	The Virtual Brain
BSP	blepharospasm	VBM	voxel-based morphometry
CD	cervical dystonia	VNS	vagus nerve stimulation
CbTC	cerebellothalamiccortical		
CT	computed tomography		
cTBS	continuous theta burst stimulation		
DBS	deep brain stimulation		
dMRI	diffusion MRI		
EEG	electroencephalography		
FDG	fluorodeoxyglucose		
FHD	focal hand dystonia		
fMRI	functional MRI		
fNIRS	functional near-infrared spectroscopy		
FTSD	focal task-specific dystonia		
GABA	gamma-aminobutyric acid		
GABAA	GABA A (i.e., GABA receptor type)		
GP	globus pallidus		
GPi	globus pallidus, internal segment		
ICA	independent components analysis		
INC	interstitial nucleus of Cajal		
LD	laryngeal dystonia		
M1	primary motor cortex		
MAN	manifesting		
MEG	magnetoencephalography		
MPTP	1-methyl-4-phenyl-1,2,3,6-tetrahydropyridine		
MRI	magnetic resonance imaging		
NIBS	noninvasive brain stimulation		
NM	non-manifesting		
PET	positron emission tomography		
PPN	pedunculopontine nucleus		
rs-fMRI	resting state functional MRI		
rTMS	repetitive TMS		
S1	primary somatosensory cortex		
SMA	supplementary motor area		